

Sonic reflection imaging in the time domain

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The model problem
in sonic imaging:
Inverse scattering

$$\frac{\partial^2 u}{\partial t^2}(x, t) = c^2(x)(\Delta u(x, t) + \delta(x - s)q(t))$$

$$g_s(x', t) = u(x', D, t) = R_s(f)(x', t)$$

$$c(x) = c_0/(1 + f(x))$$

Mammography reflection imaging

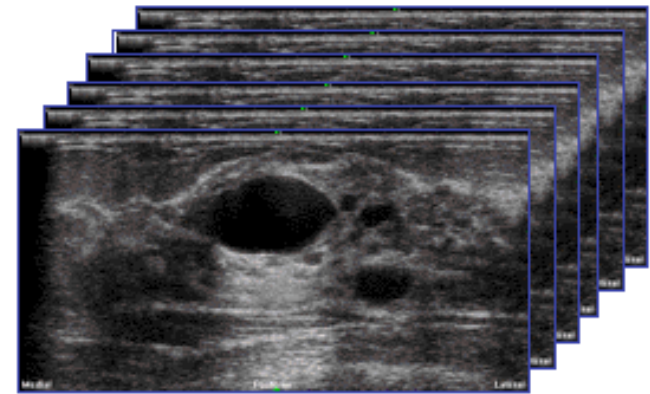
3D scanner of
U-Systems

somo•v™

Automated Breast Ultrasound View with Somo.v™



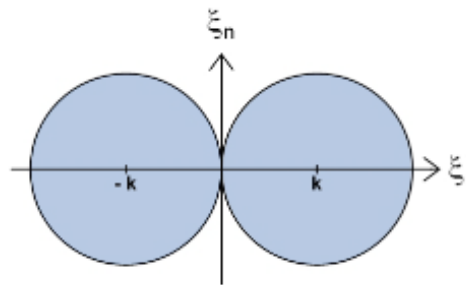
Acquisition



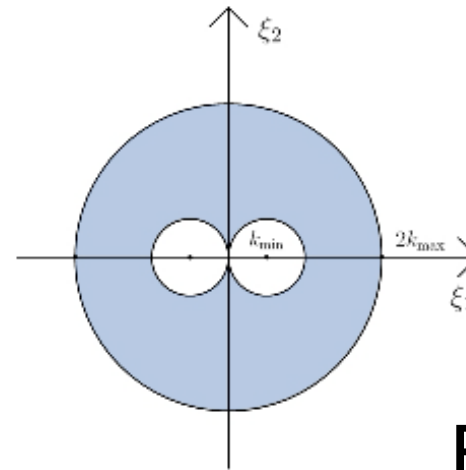
*3D Ultrasound
Data Set*



Coverage in Fourier domain



Transmission



Reflection

P. Mora , 1989

$$\hat{f}(\sigma + \rho, a(\sigma) - a(\rho)) \quad \hat{f}(\sigma + \rho, a(\sigma) + a(\rho))$$

$$a(\sigma) = \sqrt{k^2 - \sigma^2}$$

What can we do about missing low frequencies?



10 kHz - 150 kHz

Kaczmarz' method for nonlinear problems (consecutive time reversal)

Solve $R_s(f) = g_s$ for all sources s .

Update:

$$f \longleftarrow f - \alpha (R'_s(f))^* (R_s(f) - g_s)$$

$$\frac{\partial^2 z}{\partial t^2} = c^2(x) \Delta z \text{ for } x_2 > 0,$$

$$\frac{\partial z}{\partial x_2} = r \text{ on } x_2 = 0,$$

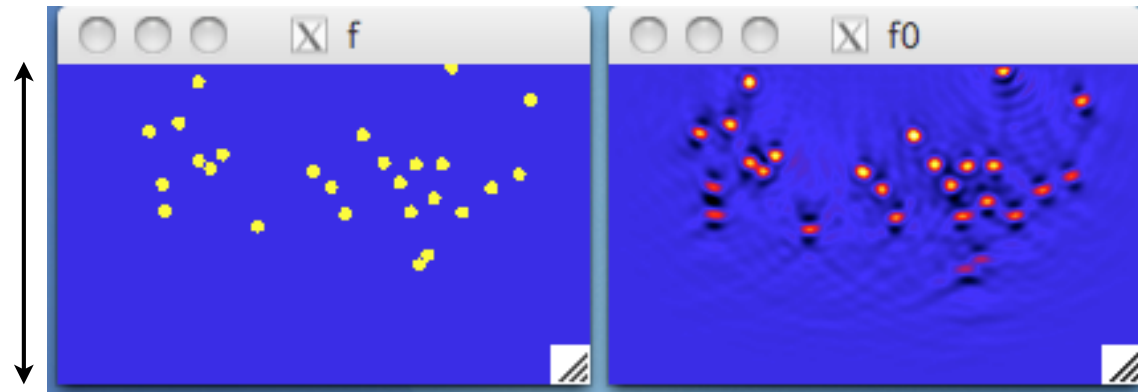
$$z = 0 \text{ for } t > T.$$

Compute the adjoint by time reversal:

$$(R'_s(f))^* r(x) = \int_0^T z(x,t) \frac{\partial^2 u(x,t)}{\partial t^2} dt$$

Easy case Nr. 1: Clutter

Original
12 cm



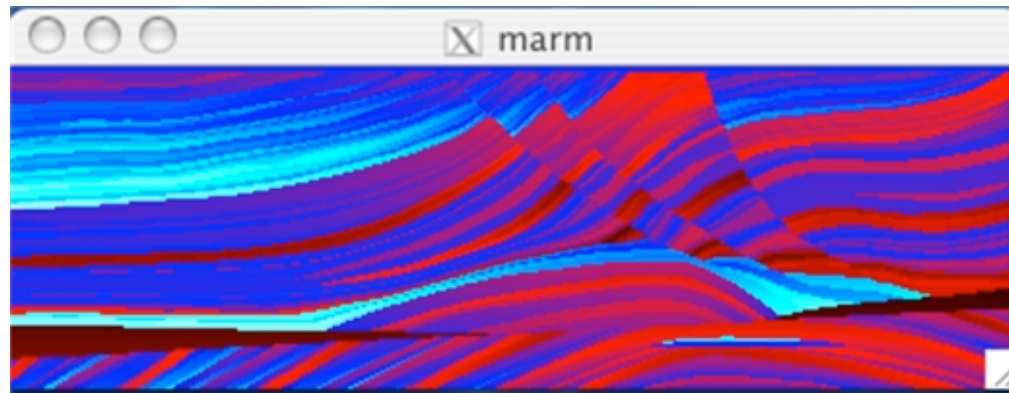
5 sweeps of
Kaczmarz

Diameter of
dots 5 mm

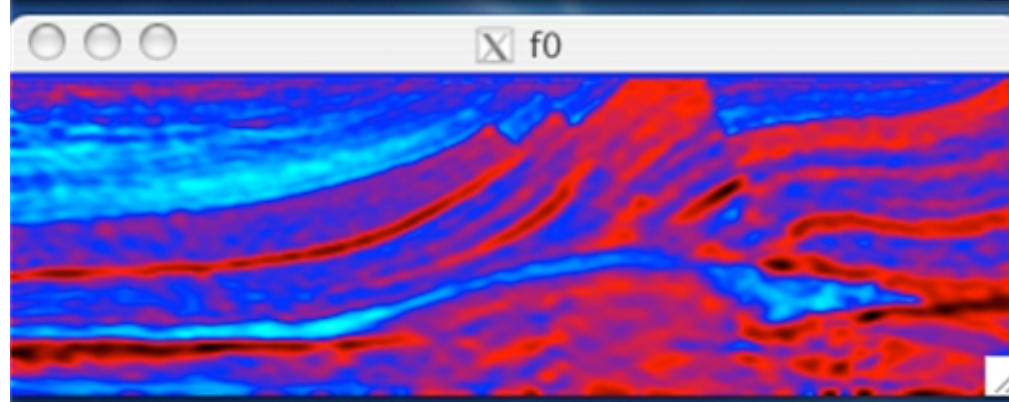
Frequency range 50 to 150 kHz
ambient speed of sound 1500m/s
wave length 1cm

Easy case Nr. 2: Source wavelet q is Gaussian peak.

Original



6 sweeps

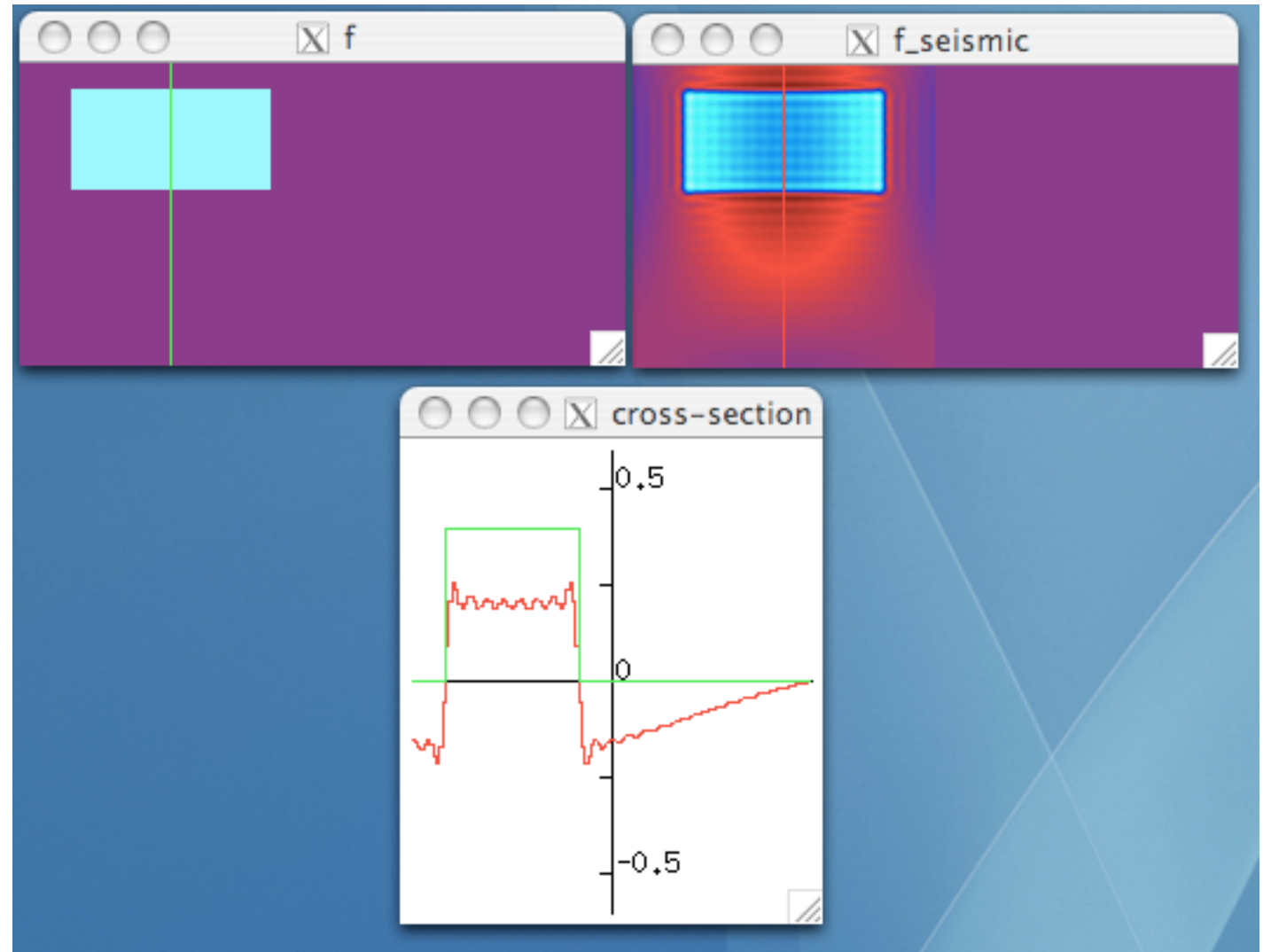


original

reconstruction

Difficult
case

10 kHz - 150 kHz



What can reflections do in mammography?

aperture 20cm

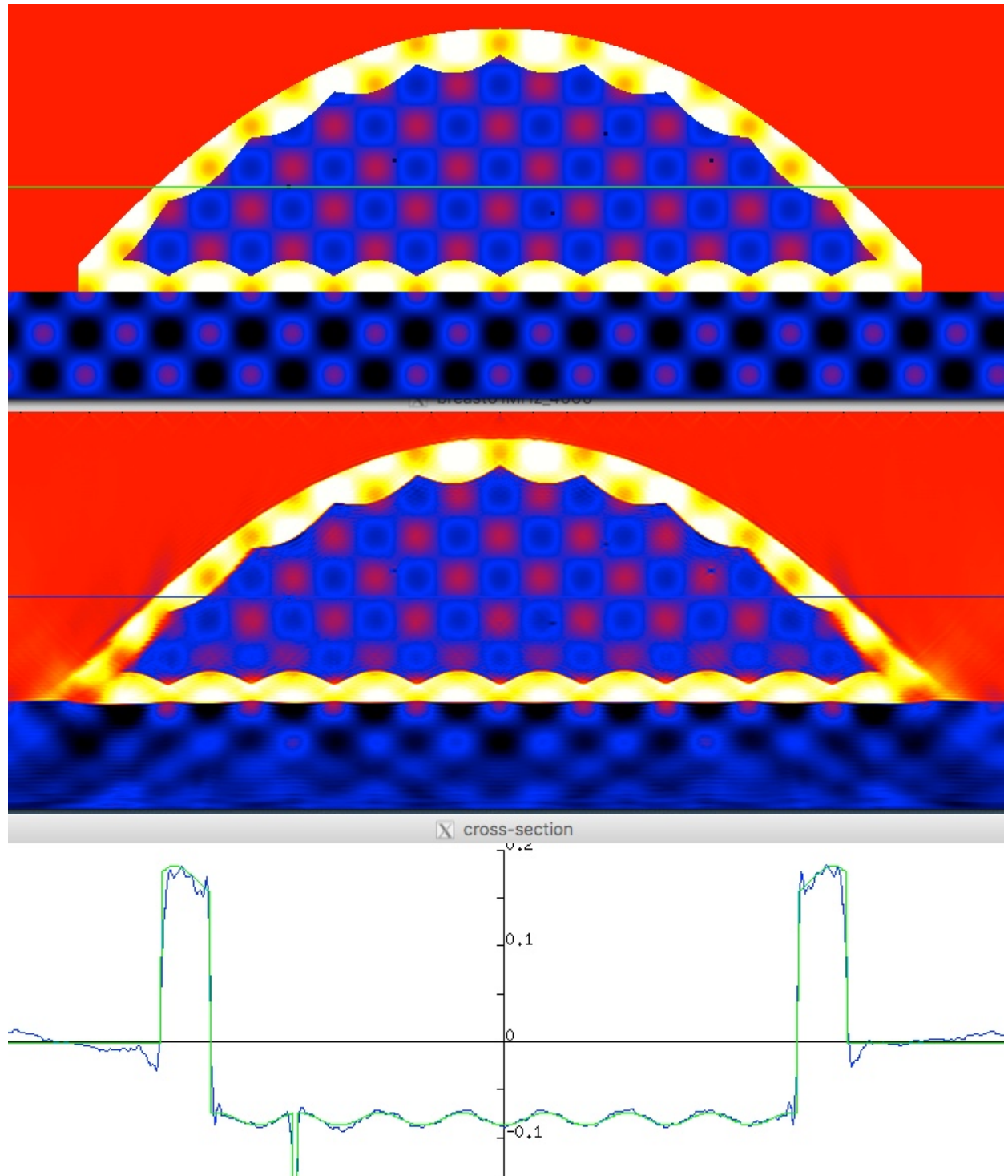
depth 5cm

frequency range
15kHz - 1MHz

wavelength 1.5 mm

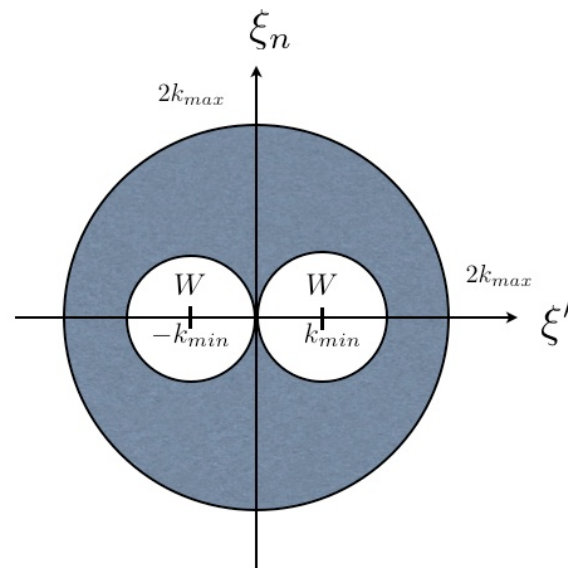
tumor 0.75 mm

stepsize 0.25 mm





Idea 1: Fill the white circles W by analytic continuation!



$$f(x) = (2\pi)^{-n/2} \int_W e^{ix \cdot \xi} \hat{f}(\xi) d\xi + (2\pi)^{-n/2} \int_{R^n \setminus W} e^{ix \cdot \xi} \hat{f}(\xi) d\xi$$

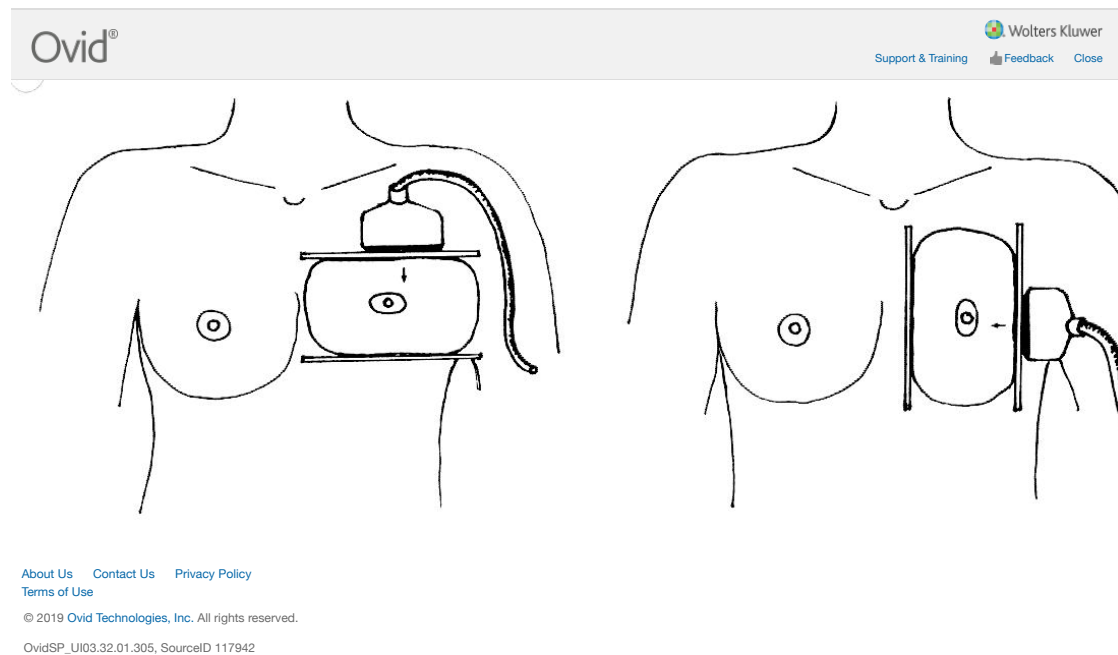
$$= \int_{|x| < r} K(x - y) f(y) dy + g(x),$$

$$K(x) = 2(2\pi)^{-n/2} \cos(kx_1) \frac{J_{n/2}(k|x|)}{(k|x|)^{n/2}}$$

Gerchberg-Papoulis

Idea 2: Use reflector

CARI (K. Richter, 1996)
Clinical amplitude/velocity reconstructive imaging
H. Madjar (2018)
Challenges in Breast Ultrasound



The model problem with a reflector

$$\frac{\partial^2 u}{\partial t^2}(x, t) = c^2(x)(\Delta u(x, t) + \delta(x - s)q(t))$$

$$g_s(x', t) = u(x', D, t) = R_s(f)(x', t)$$

$$\frac{\partial u}{\partial x_n}(x', 0, t) = 0$$

Born approximation

$G(x, y)$ free space Green's function

$G_0(x, y)$ Green's function for reflector, $x = (x', x_n), y = (y', y_n) :$

$$G_0(x, y) = G(x' - y', x_n - y_n) + G(x' - y', x_n + y_n)$$

$$\tilde{u}(x) - \tilde{u}_0(x) = k^2 \tilde{q}(\omega) \int_{0 < y_n < D} G_0(x, y) f(y) \tilde{u}_0(y) dy, k = \omega/c_0$$

Plane wave decomposition of Green's function

$$\hat{G}(\xi', x_n) = i(2\pi)^{(n-1)/2} c_n \frac{e^{i|x_n|a(\xi')}}{a(\xi')},$$

$$a(\xi') = \sqrt{k^2 - |\xi'|^2}, c_2 = 1/(4\pi), c_3 = 1/(8\pi^2)$$

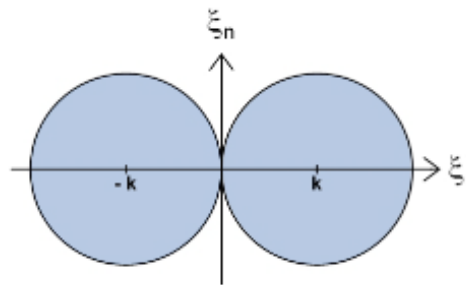
Resulting integral equation:

$$data(\rho, \sigma) = (C\hat{f})(\rho + \sigma, a(\rho) + a(\sigma)) + (C\hat{f})(\rho + \sigma, a(\rho) - a(\sigma))$$

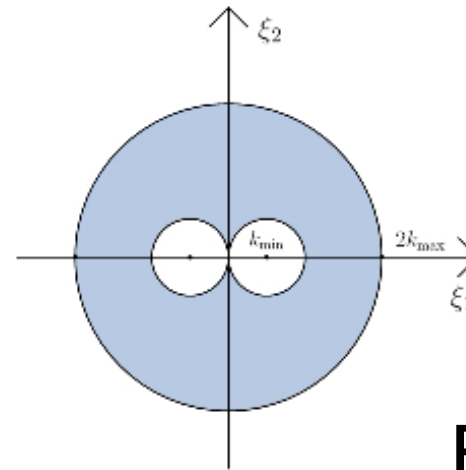
$\hat{f}$ n -dimensional Fourier-transform of f , $|\rho|, |\sigma| \leq k$

C Cosine-transform with respect to last argument

Coverage in Fourier domain



Transmission



Reflection

P. Mora , 1989

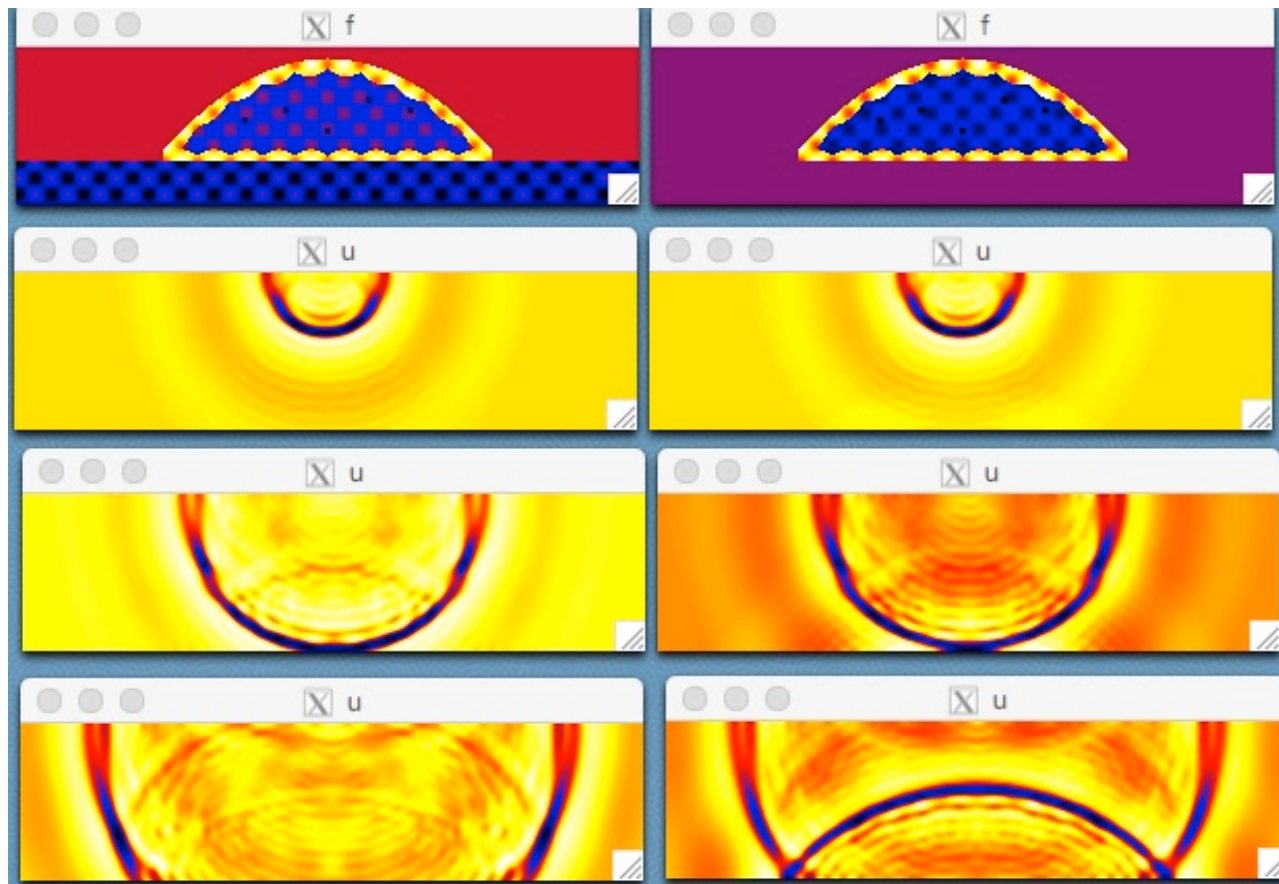
$$\hat{f}(\sigma + \rho, a(\sigma) - a(\rho)) \quad \hat{f}(\sigma + \rho, a(\sigma) + a(\rho))$$

$$a(\sigma) = \sqrt{k^2 - \sigma^2}$$

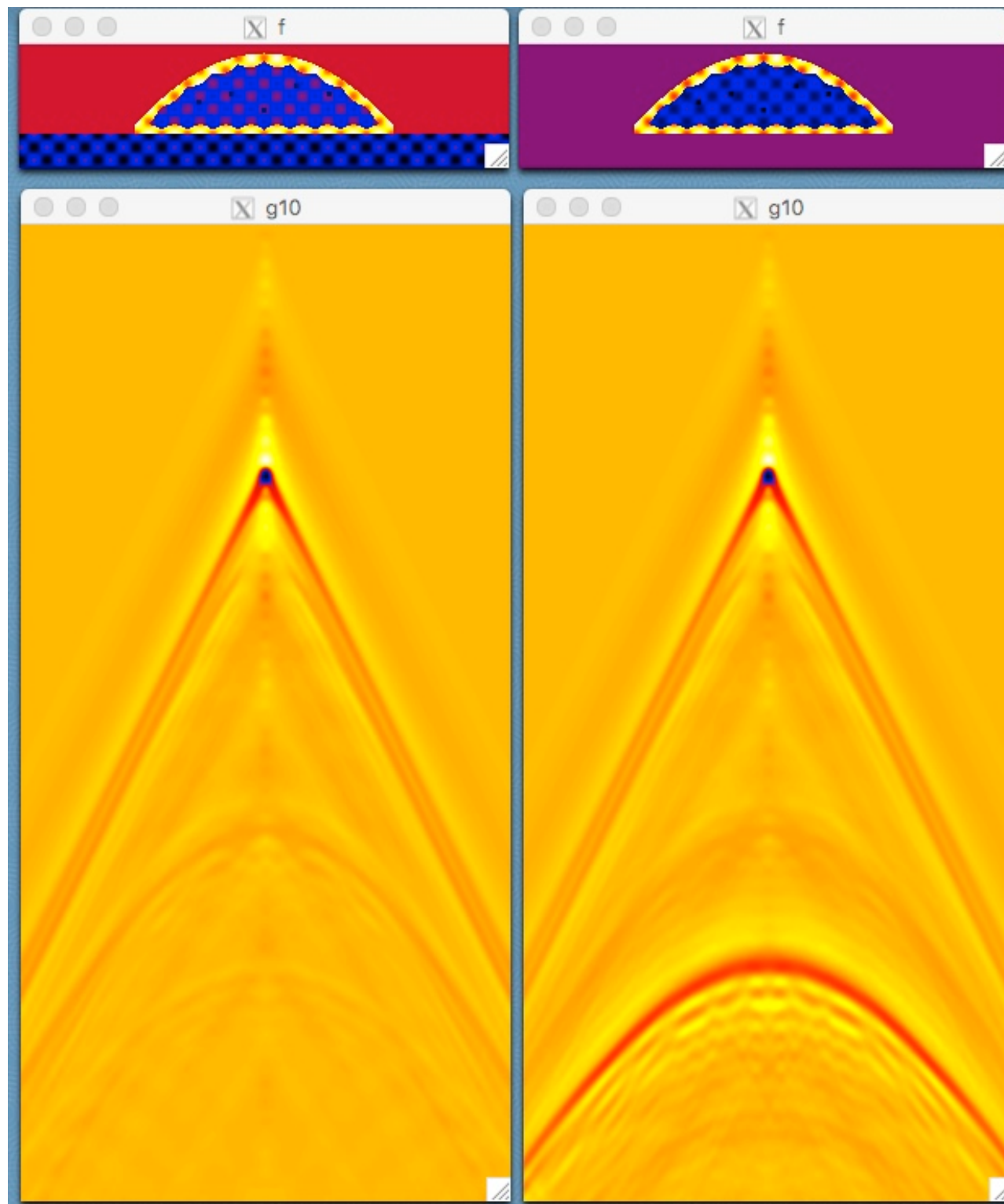
Waves from 1 source on the top boundary

No reflector

Reflector

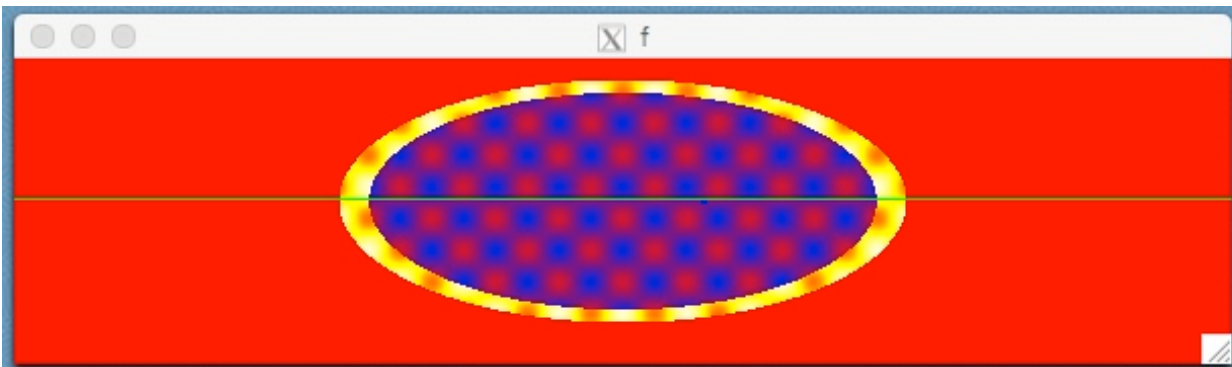


**Data without
reflector**

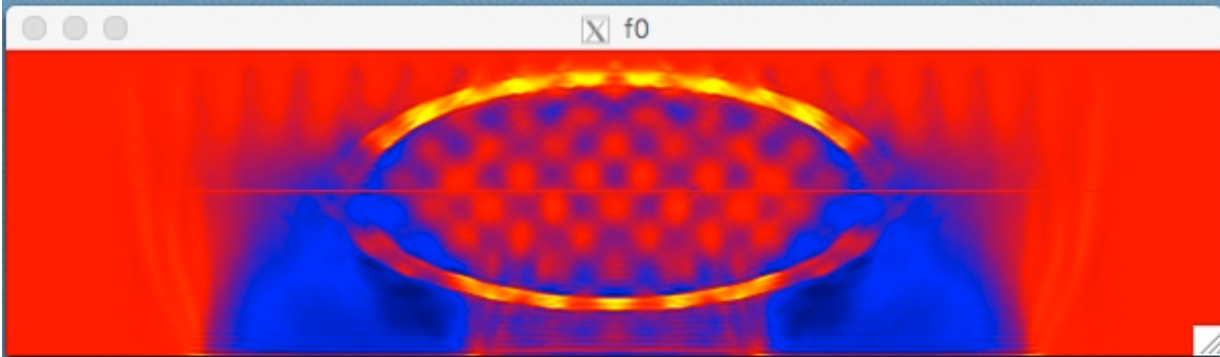


**Data with
reflector**

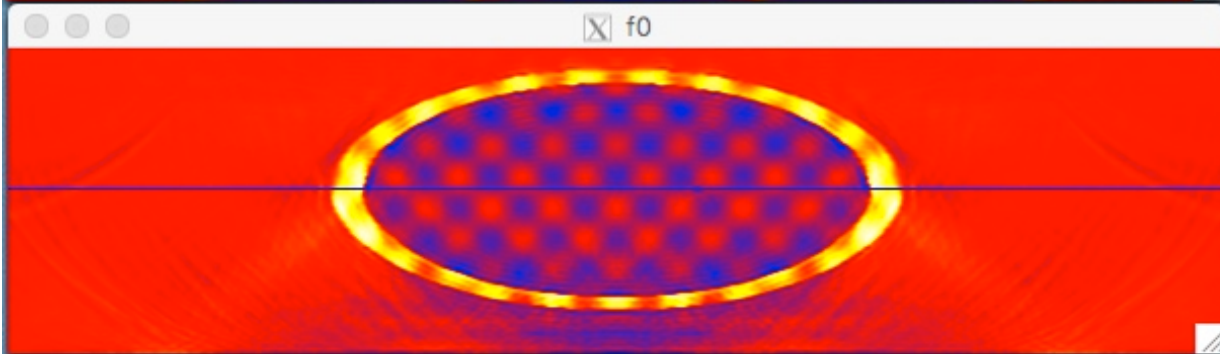
**original
tumors 1.5 mm**



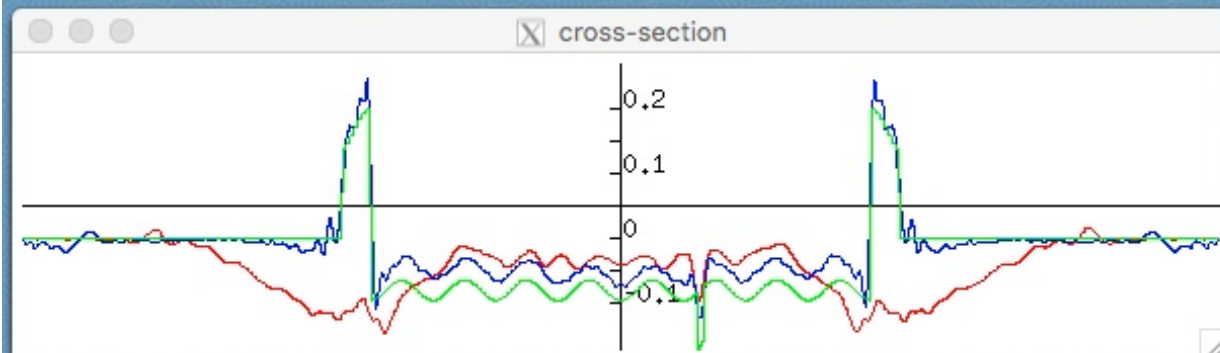
**reconstruction
without reflector
30-500 kHz**



**reconstruction
with reflector
30-500 kHz**



cross sections





Layered medium

$$f(x_1, x_2) = f(x_2).$$

Born approximation, one source at $x_1 = 0$, $x_2 = 0$:

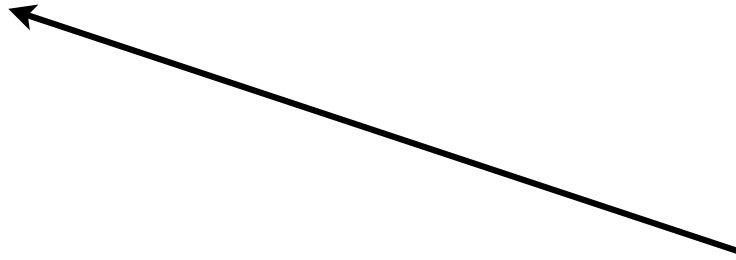
$$g_k(x) = (2\pi)^{-1/2} \int e^{-ix\xi} \hat{f}(-2\kappa(\xi)) d\xi, \quad \kappa = \sqrt{k^2 - \xi^2}.$$

Finite aperture: Data available for $|x| \leq A$ only.

All we can determine: $\int \delta_A(\eta - \xi) \hat{f}(-2\kappa(\xi)) d\xi$, $\delta_A(\xi) = \frac{A}{\pi} \text{sinc}(A\xi)$.

Determine $\hat{f}$ from

$$\int \delta_A(\eta - \xi) \hat{f}(-2\kappa(\xi)) d\xi, \quad \delta_A(\xi) = \frac{A}{\pi} \text{sinc}(A\xi), \quad \kappa = \sqrt{k^2 - \xi^2}.$$



peaks in η , bandwidth A

for line object at depth z :

$\hat{f}(-2\kappa(\xi))$ can be stably

$$f(x) = \delta(x - z), \quad \hat{f}(\xi) \sim e^{-iz\xi},$$

determined for $A > 2z|\xi|/\kappa(\xi)$

$$\hat{f}(-2\kappa(\xi)) \sim e^{-2iz\kappa(\xi)} \quad \text{for } |\xi| < k.$$

$$\text{i.e. } \frac{2k}{\sqrt{1 + A^2/4z^2}} < 2\kappa < 2k.$$

$$\text{bandwidth } 2z|\kappa'(\xi)| = 2z|\xi|/\kappa(\xi)$$

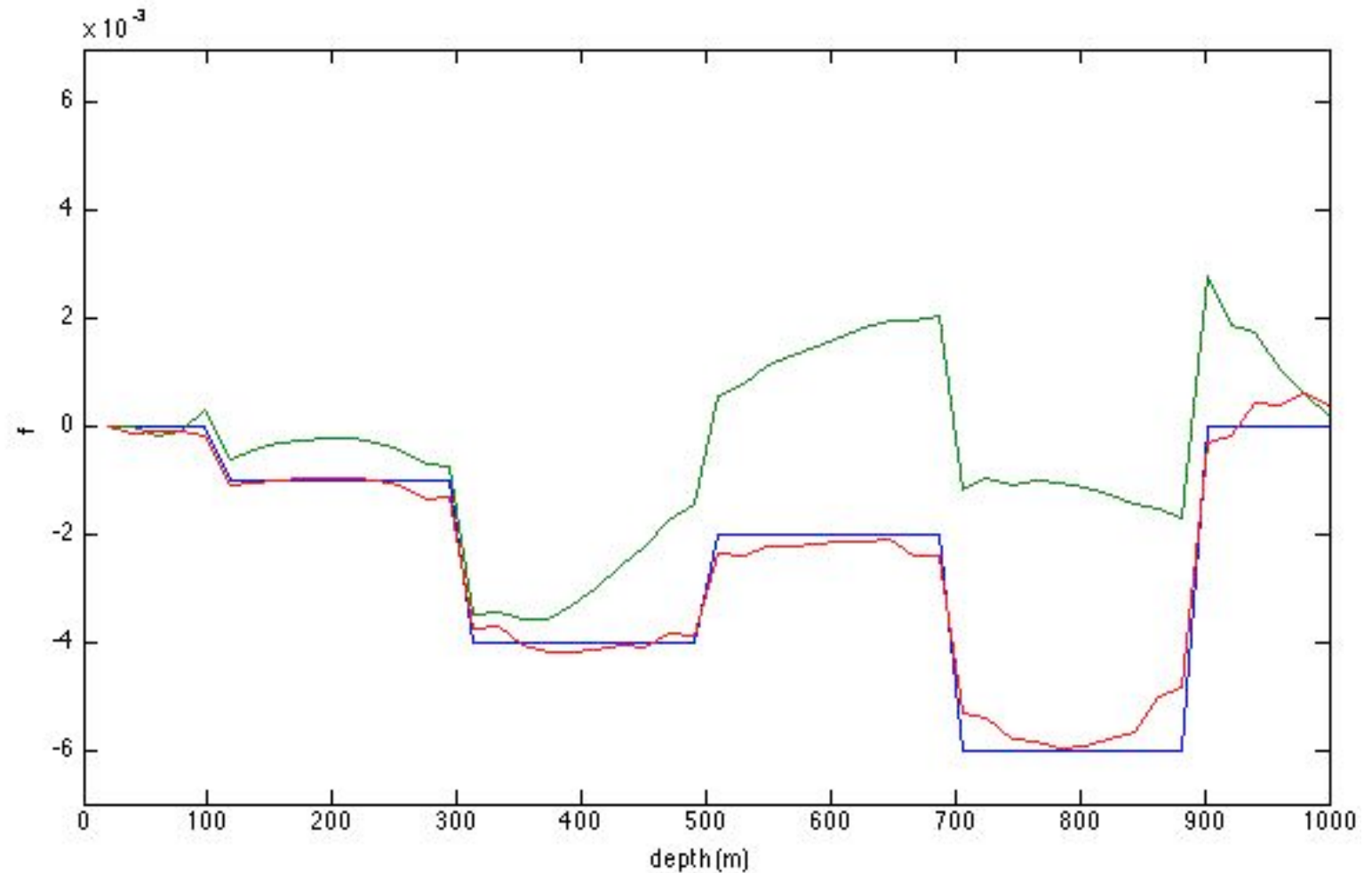
Sirgue & Pratt 2004

Kaczmarz' method, frequencies 5-25 Hz

— true profile

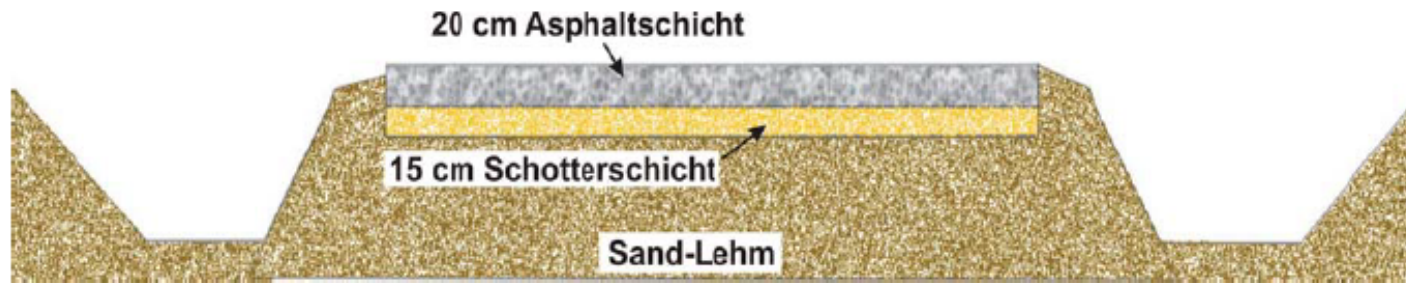
— Kaczmarz
starting
at $f=0$

— Kaczmarz
with
analytic
continuation

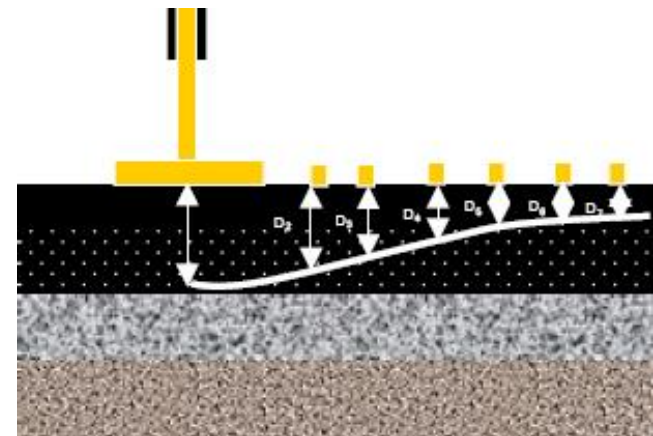


aperture 12 km, wave length 400 m

BASt



Falling weight deflectometer (FWD)



Conclusion:

Reflection imaging without low frequencies can be improved by

reflectors

big apertures

analytic continuation