

# Diffuse optical imaging of biological tissue

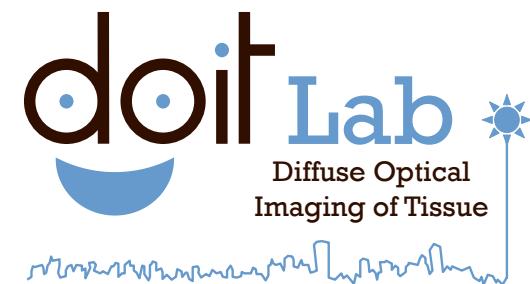
Sergio Fantini,

Angelo Sassaroli, Thao Pham, Giles Blaney, Cristianne Fernandez

*Department of Biomedical Engineering  
Tufts University*



Conference on **Modern Challenges in Imaging**  
In the Footsteps of Allan MacLeod Cormack  
On the Fortieth Anniversary of his Nobel Prize



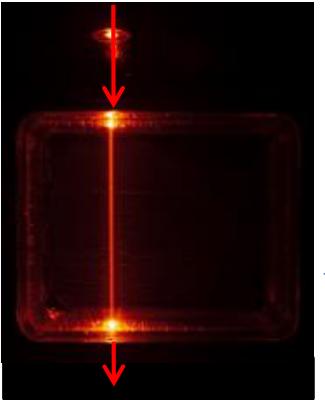
August 5-9, 2019, Tufts University, Medford, MA

# Outline

- **Diffuse optical imaging:**
  - Breast cancer imaging
  - Functional brain imaging
- **New approach to enhance depth sensitivity in diffuse optical imaging**



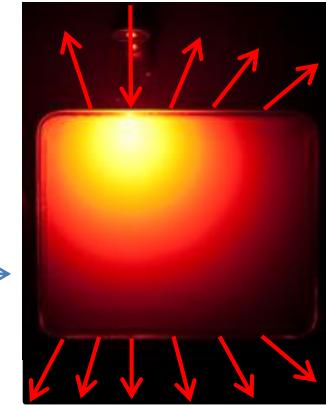
No/weak scattering



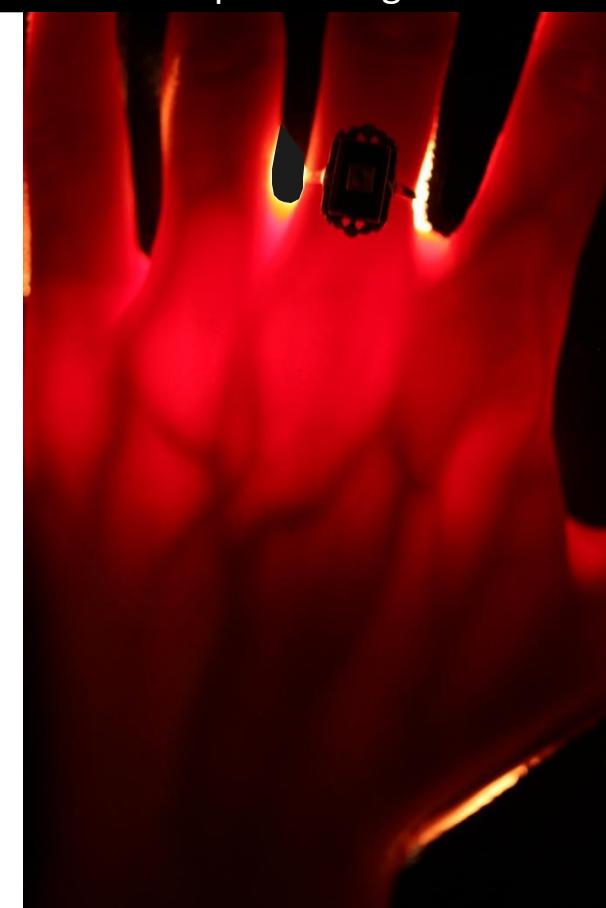
X-ray image of a hand



Strong scattering



Diffuse optical image of a hand



Year: 2020

# Optical Mammography

- Response to neoadjuvant therapy;
  - Photo-acoustics
- 
- Time-resolved methods;
  - Broadband spectroscopy;
  - Optical tomography;
  - Co-registrations;
  - Photo-acoustics;
  - Optical contrast agents;
  - New commercial systems



**Multicenter clinical study**  
Alveryd et al., Cancer 65, 1671 (1990).

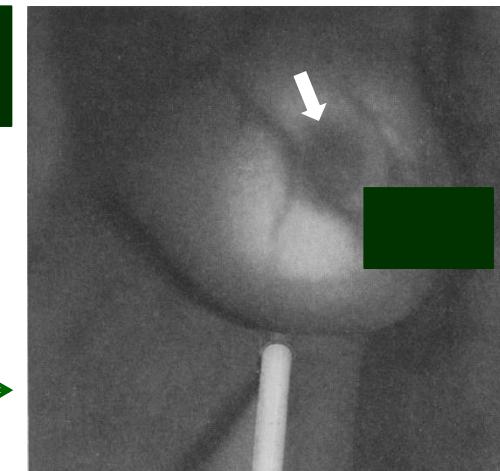
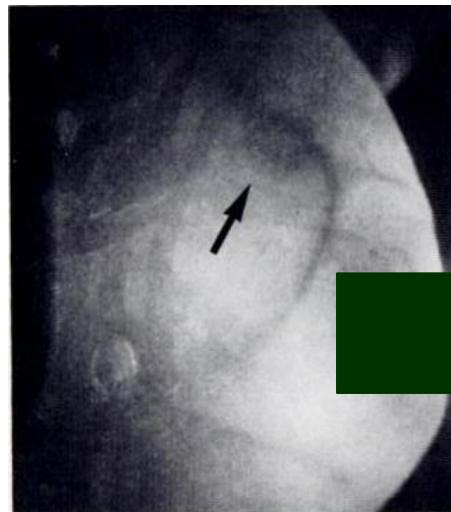
“The study shows that lightscanning in its current form is inferior to standard mammography.”

**Pilot clinical studies**  
Bartrum and Crow, AJR 142, 409(1984).

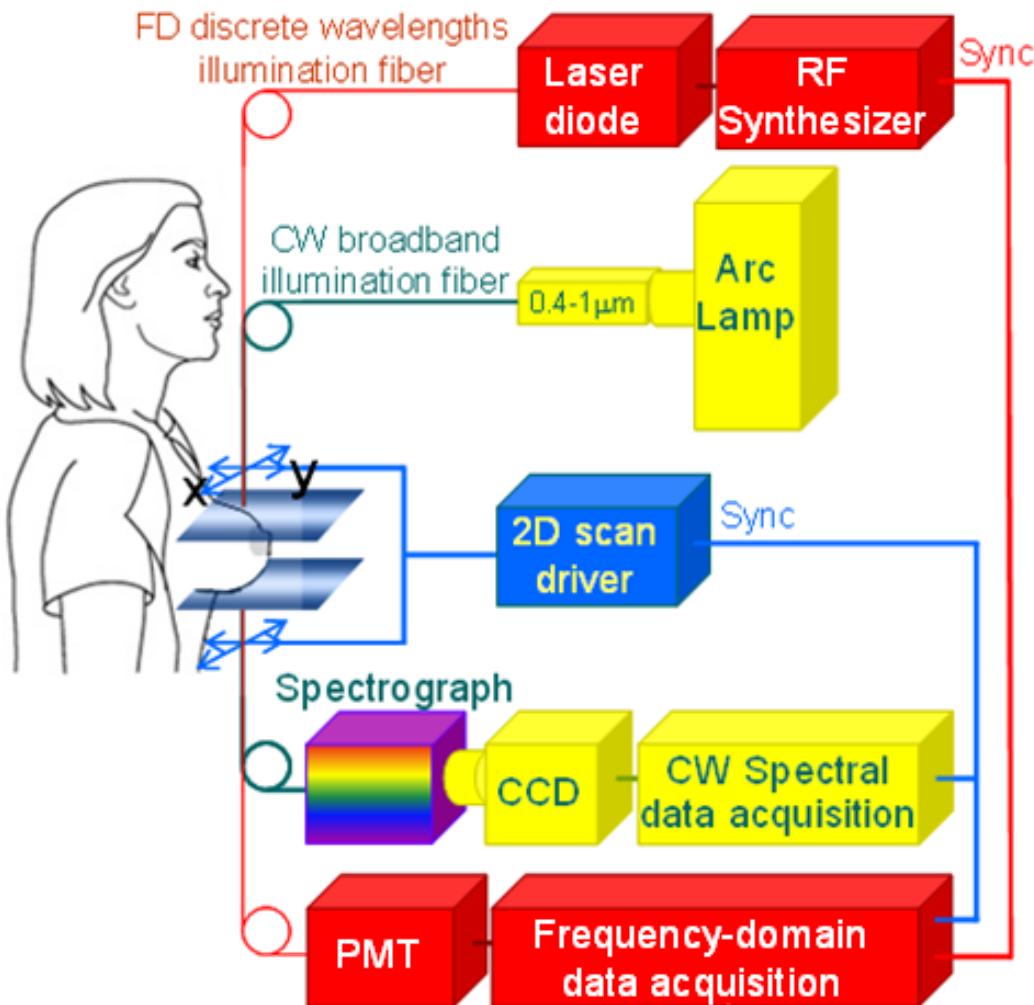
**Lightscanning**  
Carlsen, Diagn. Imaging 4, 28 (1982).

**Diaphanography**  
Gros, Radiol. Electrol. 53, 297 (1972).

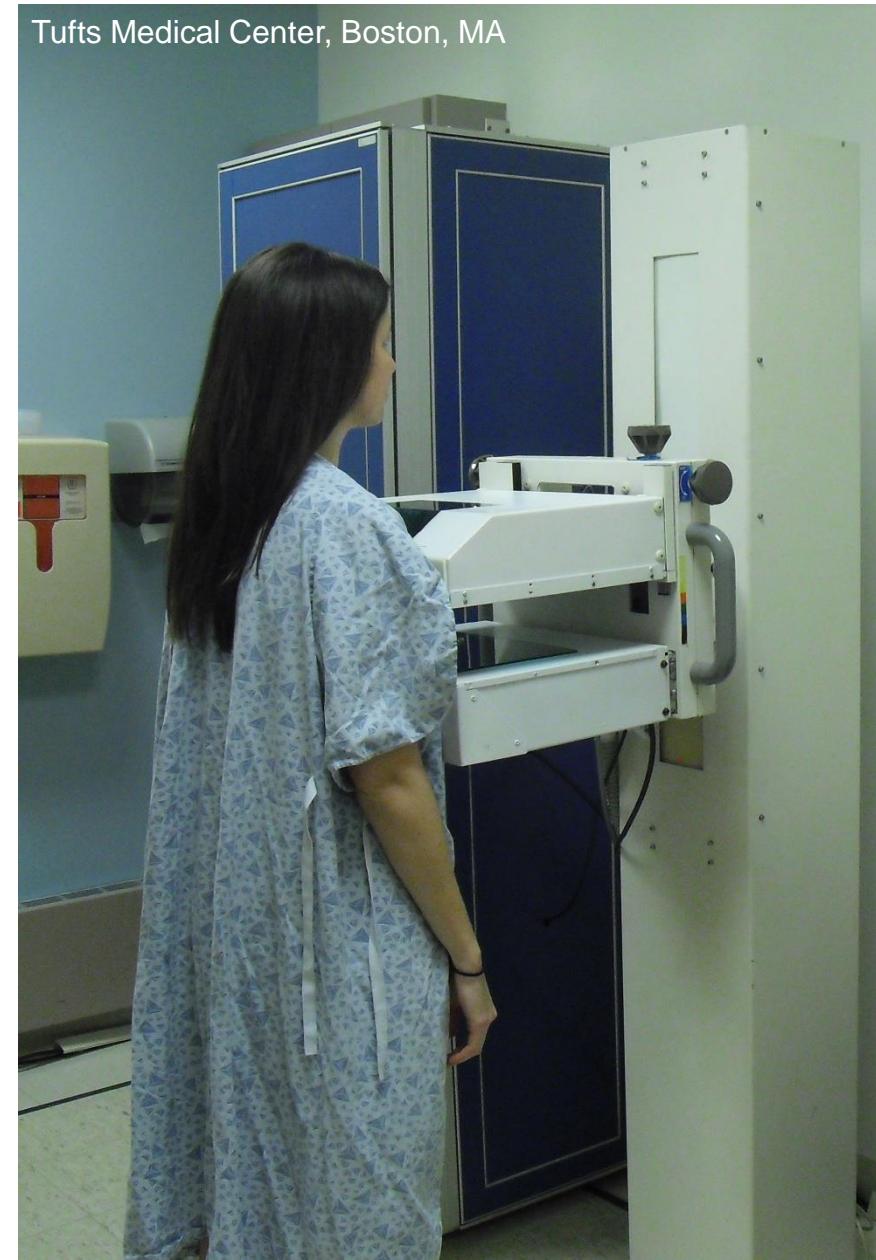
**Breast transillumination**  
Cutler, Surg. Gynecol. Obstet. 48, 721 (1929).  
(Currently: J. Am. Coll. Surg.)



# Optical mammography at Tufts



[Yang Yu et al., Appl. Opt. 48, D225 (2009).]

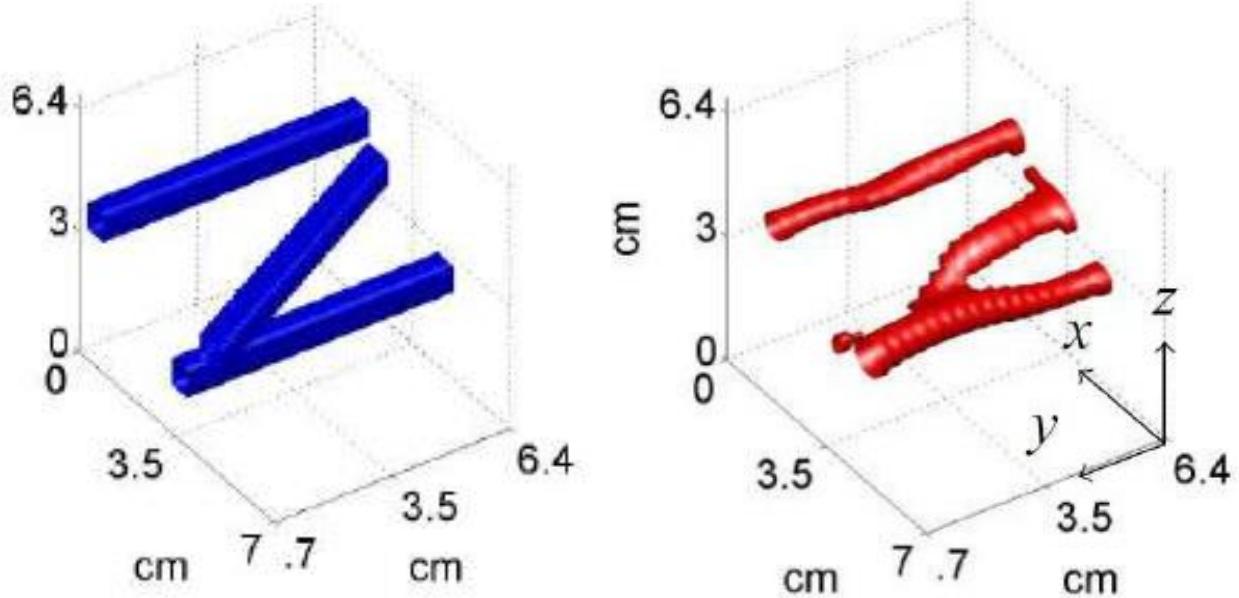


# Parametric estimation of 3D tubular structures for diffuse optical tomography

Fridrik Larusson,<sup>1,4,\*</sup> Pamela G. Anderson,<sup>2</sup> Elizabeth Rosenberg,<sup>2</sup>  
Misha E. Kilmer,<sup>3</sup> Angelo Sassaroli,<sup>2</sup> Sergio Fantini,<sup>2</sup>  
and Eric L. Miller<sup>1</sup>



[Biomed. Opt. Express **4**, 271 (2013).]



Ground truth and reconstruction results with a parametric level set method (PaLS) using two detectors for each source location and inter-slice regularization.

SIAM J. SCI. COMPUT.  
Vol. 37, No. 5, pp. B712–B743

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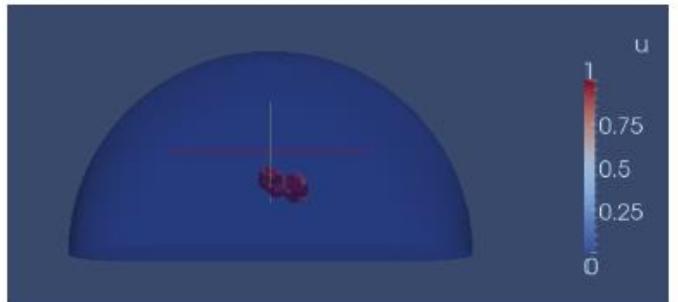
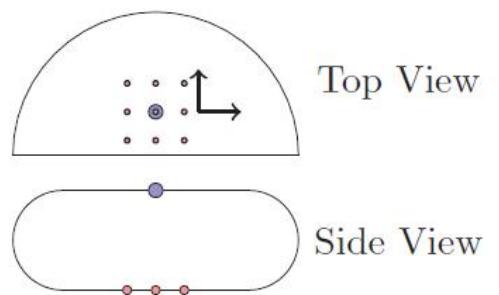
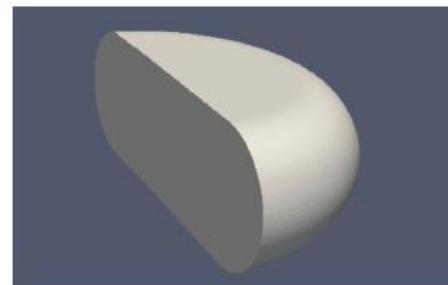
## FAST ALGORITHMS FOR HYPERSPECTRAL DIFFUSE OPTICAL TOMOGRAPHY\*

ARVIND K. SAIBABA<sup>†</sup>, MISHA KILMER<sup>‡</sup>, ERIC L. MILLER<sup>†</sup>, AND SERGIO FANTINI<sup>§</sup>



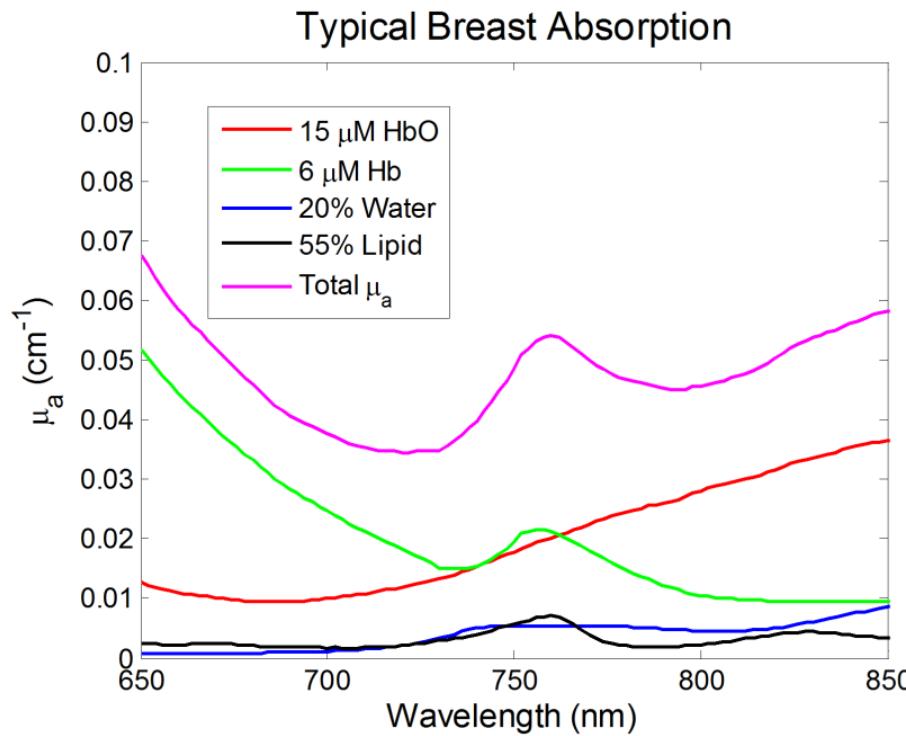
[SIAM J. Sci. Comput. **37**, B712 (2015).]

Reconstruction of chromophore concentrations and shape of a localized perturbation in a breast-like phantom using the Born approximation.



# Breast tissue: Absorption and scattering spectra

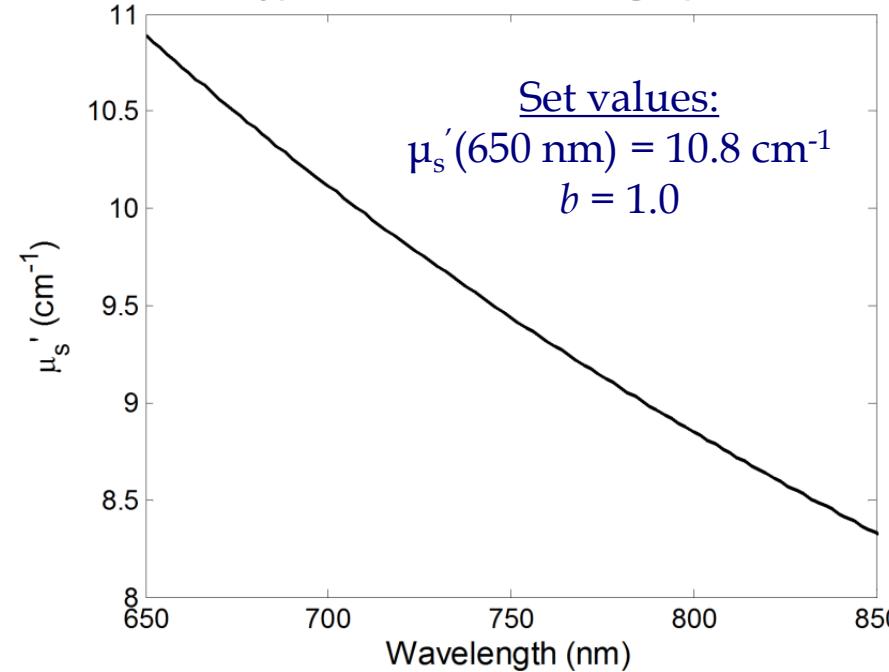
$$\mu_a(\lambda) = \varepsilon_{\text{HbO}}(\lambda) [\text{HbO}] + \varepsilon_{\text{Hb}}(\lambda) [\text{Hb}] \\ + \varepsilon_{\text{water}}(\lambda) [\text{water}] + \varepsilon_{\text{lipid}}(\lambda) [\text{lipid}]$$



[Grosenick et al., Phys. Med. Biol. **50**, 2451 (2005)]

$$\mu_s'(\lambda) = \mu_s'(\lambda_0) \left( \frac{\lambda}{\lambda_0} \right)^{-b}$$

Typical Breast Scattering Spectra



Transmission spectra modeled in each pixel with diffusion theory (slab geometry, extrapolated boundary conditions)

Known	Fixed	Found
$T(\lambda)$	$\{\varepsilon_i(\lambda), L\}$	$\mu_s'(\lambda_0), b, [\text{Hb}], [\text{HbO}], [\text{water}], [\text{lipid}]$



# Pilot clinical study on 26 patients with breast cancer

In collaboration with Tufts  
Medical Center:  
Dr. Roger Graham  
Dr. Marc Homer  
Dr. Shital Makim



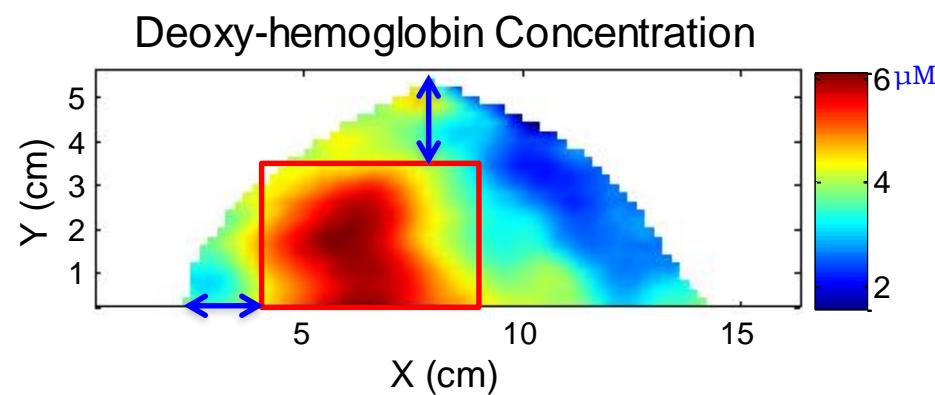
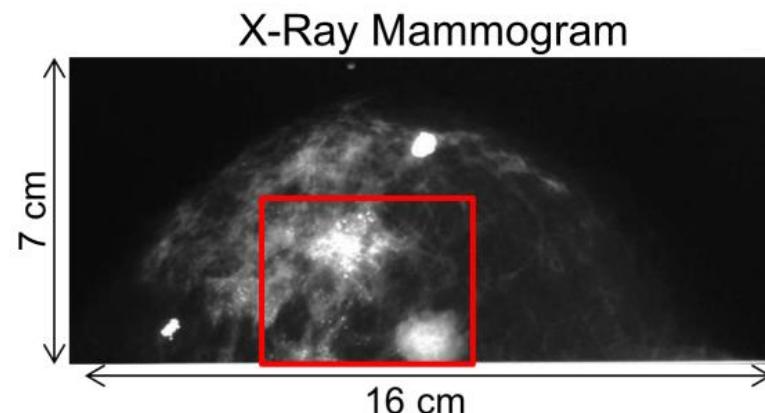
[Pami Anderson et al., PloS ONE 10, e0117322 (2015)]

Number of Patients	26
Age (years)	
Average	57
Std	11
Range	36-76
Tumor Size (cm)	
Average	2.0
Std	1.4
Range	0.5-5.5
Cancer Type (# patients)	
DCIS	3
IDC	6
IDC/DCIS	12
IDC/DCIS/LCIS	2
ILC	1
ILC/LCIS	2



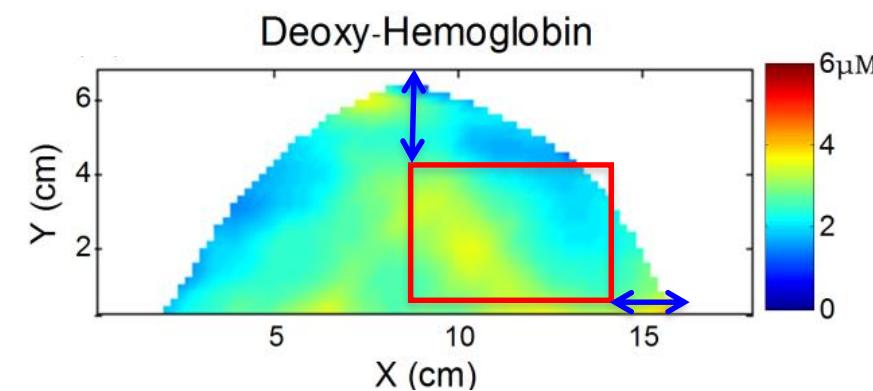
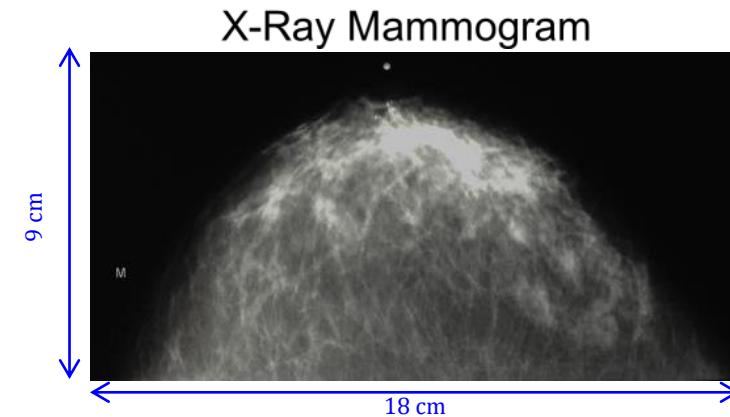
# Patient #15

LCC  
Cancerous Breast



$$\Delta \text{Hb} = 2.2 \pm 0.8 \mu\text{M}$$

RCC  
Healthy Breast

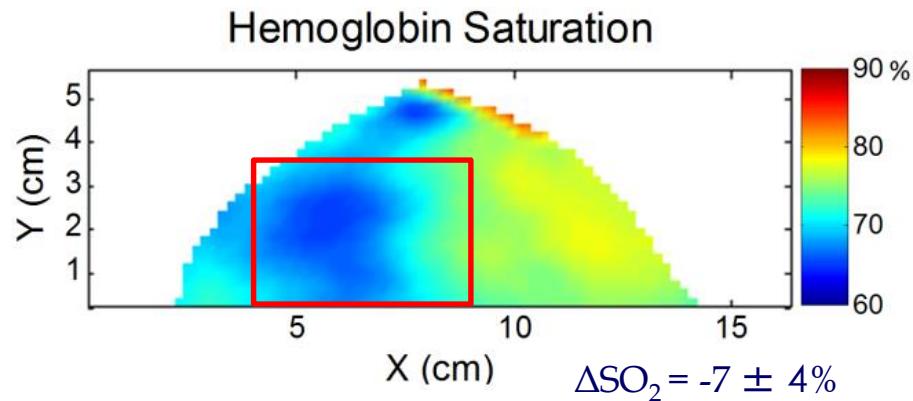


$$\Delta \text{Hb} = 0.3 \pm 0.7 \mu\text{M}$$

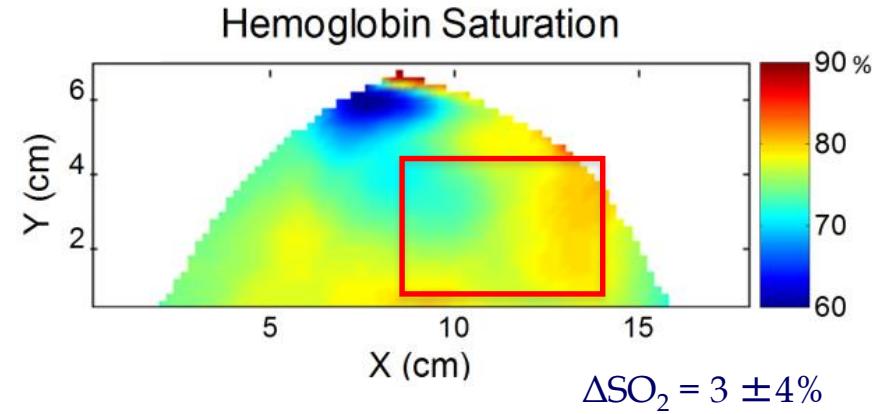


# Patient #15

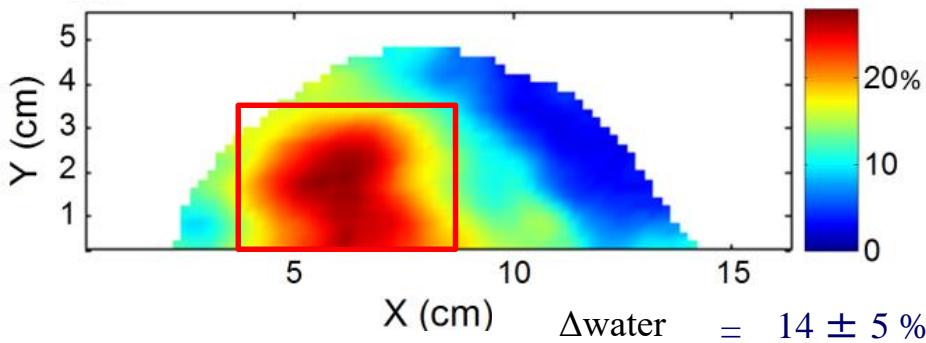
LCC - Cancerous Breast



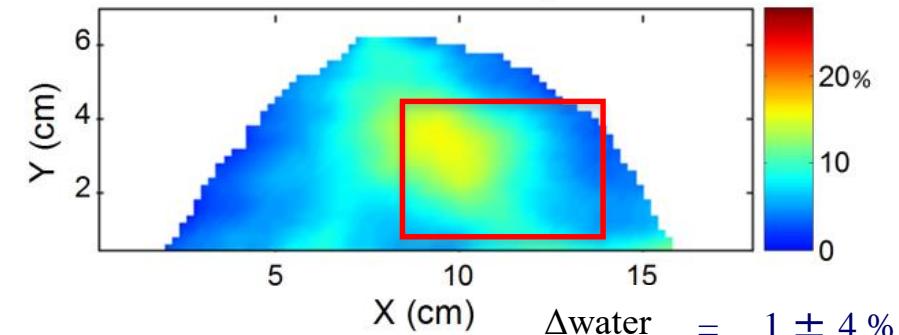
RCC - Healthy Breast



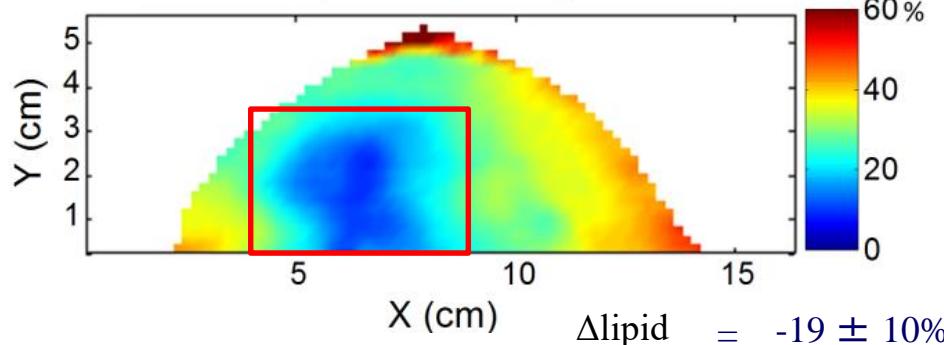
Water Percentage



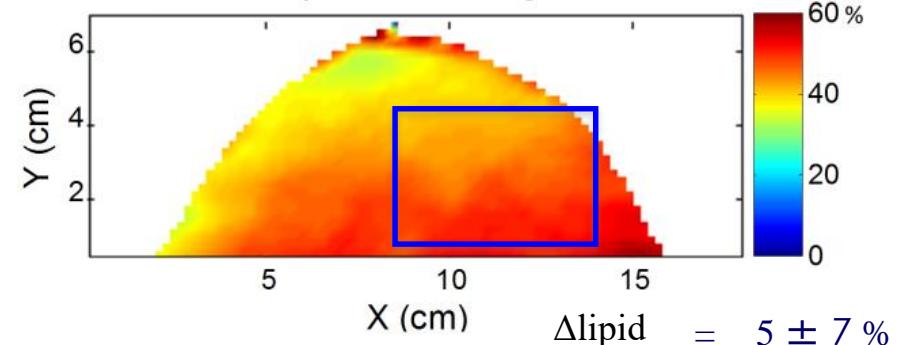
Water Percentage



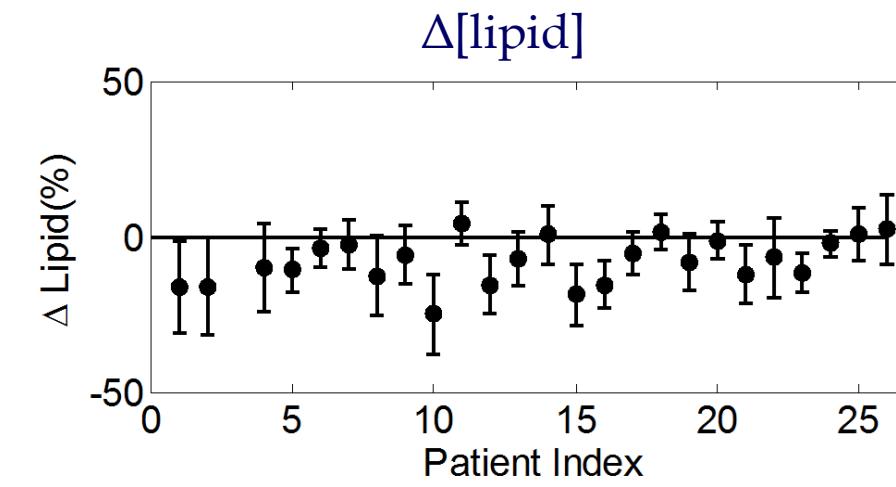
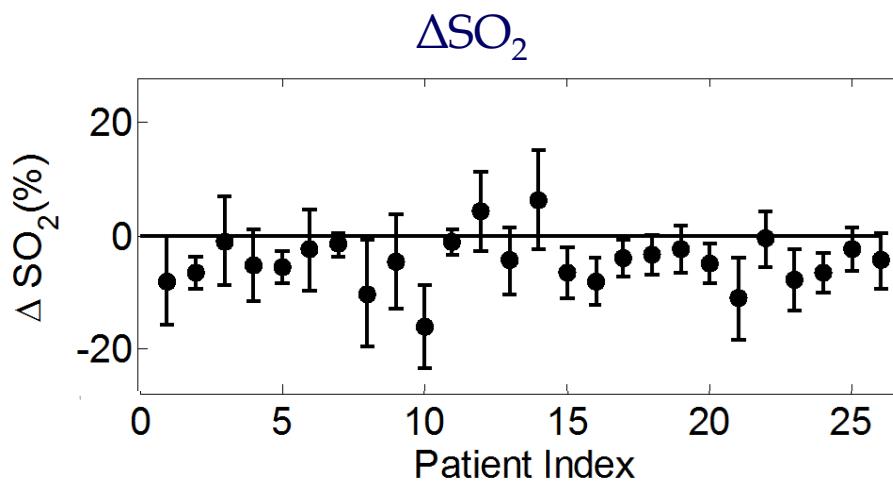
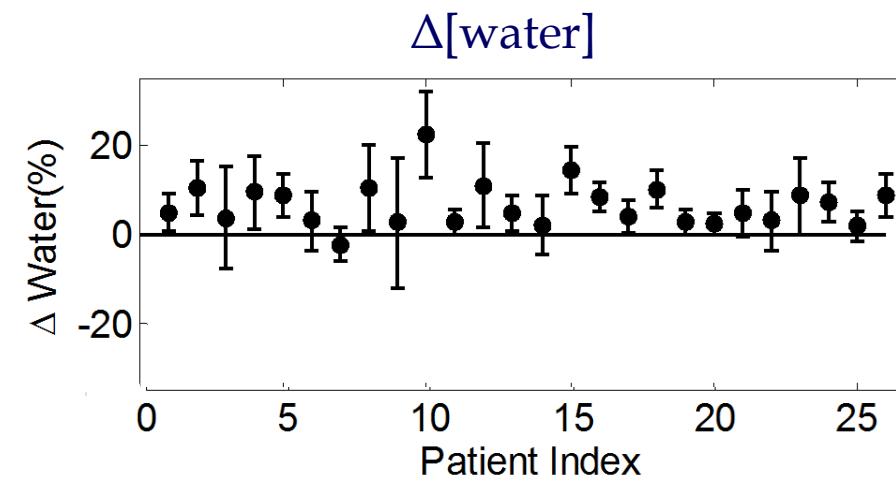
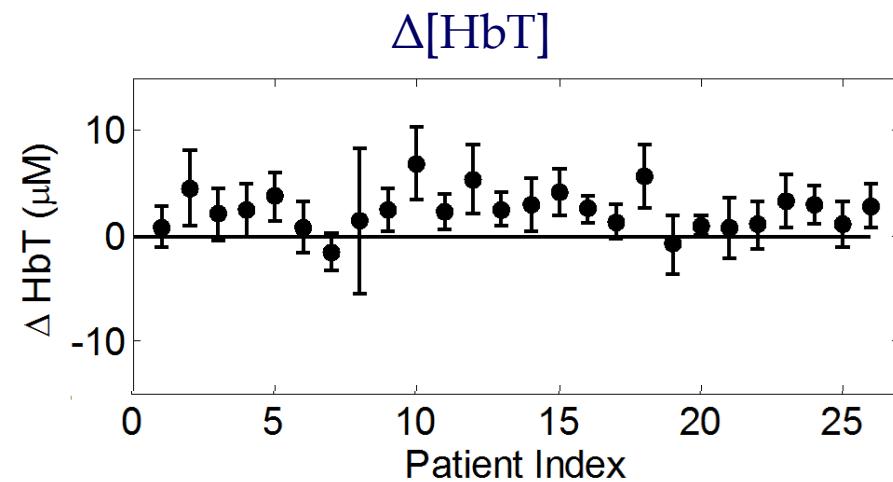
Lipid Percentage



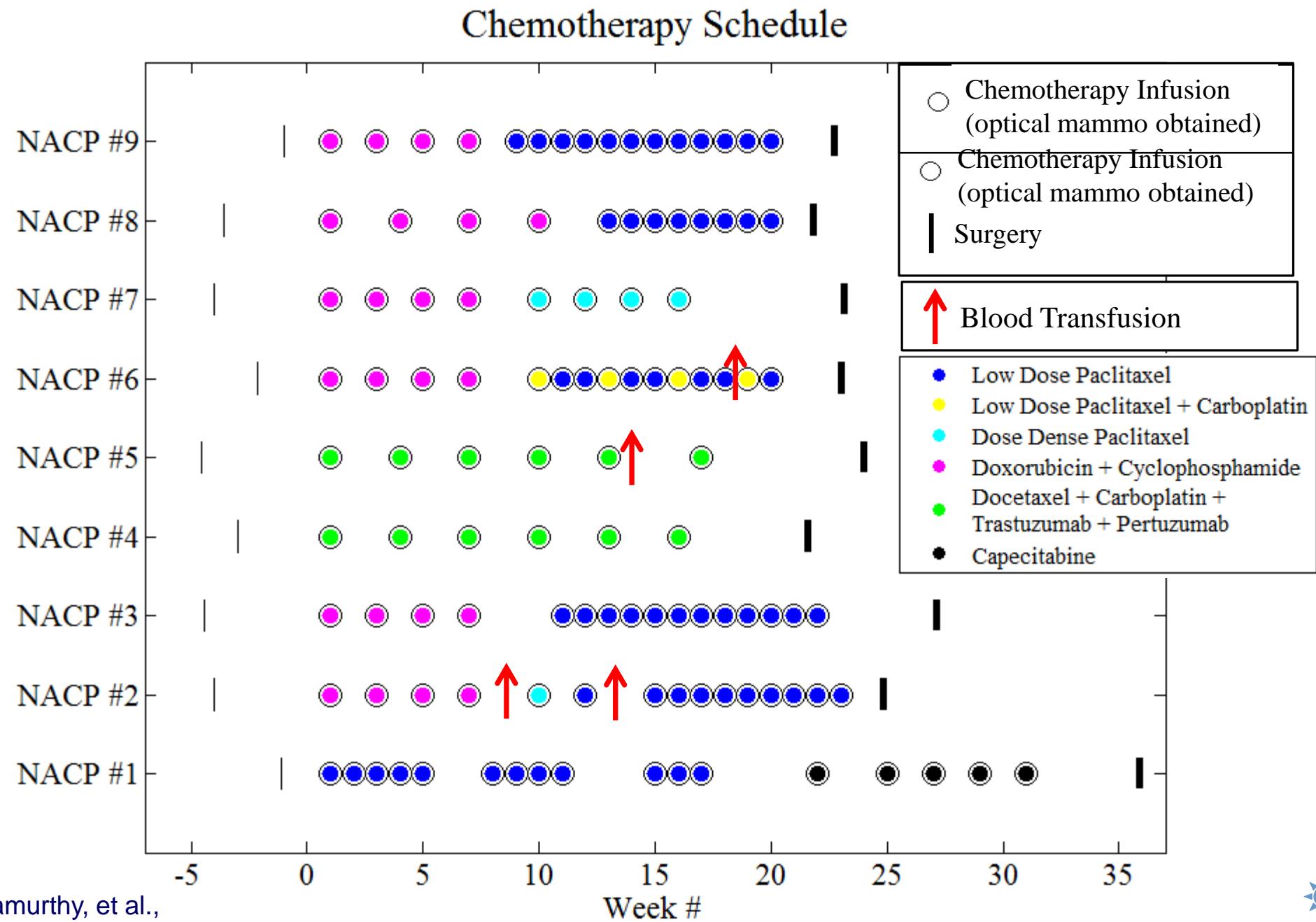
Lipid Percentage



# Results on all 26 patients



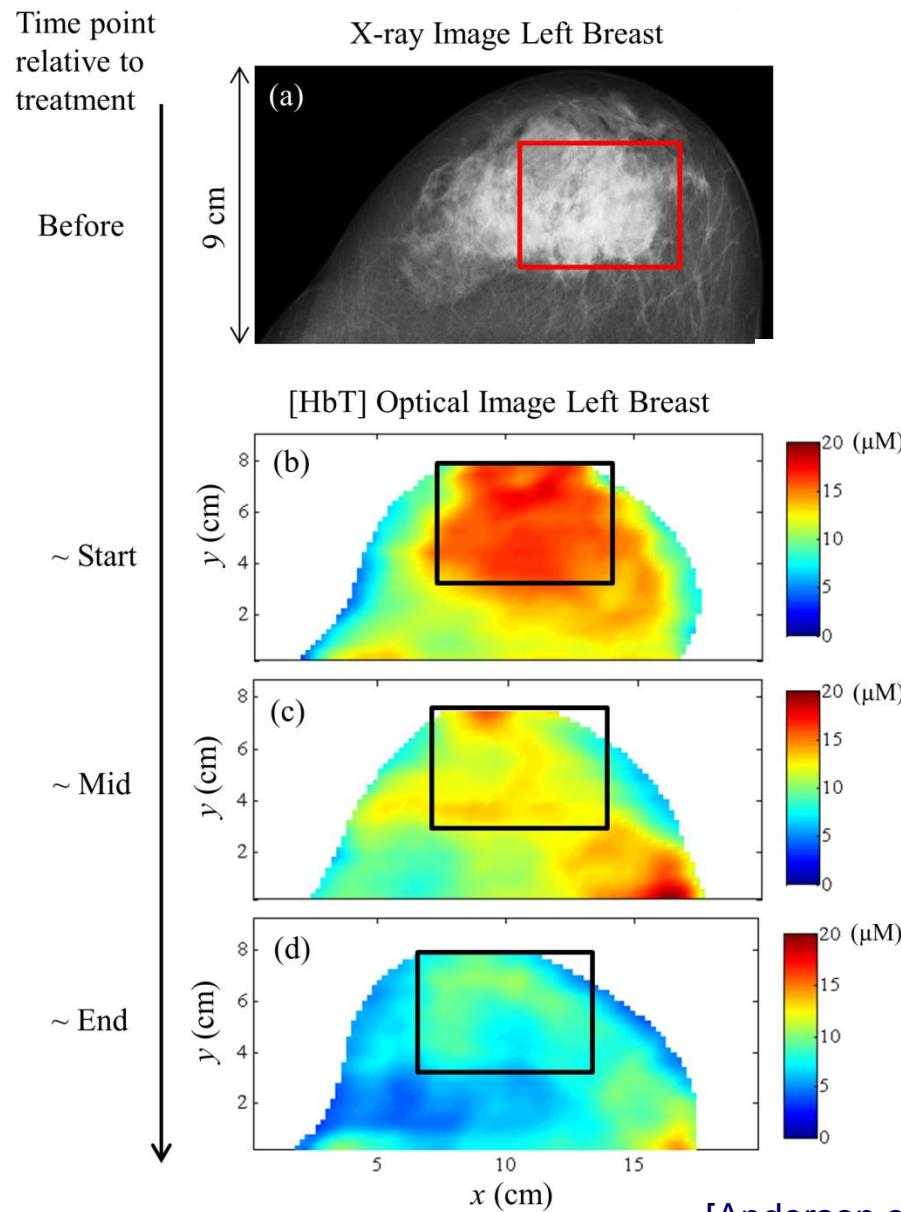
# Individual response to neoadjuvant chemotherapy



[Pami Anderson, Nishanth Krishnamurthy, et al.,  
Acad. Radiol. 24, 1240 (2017)]

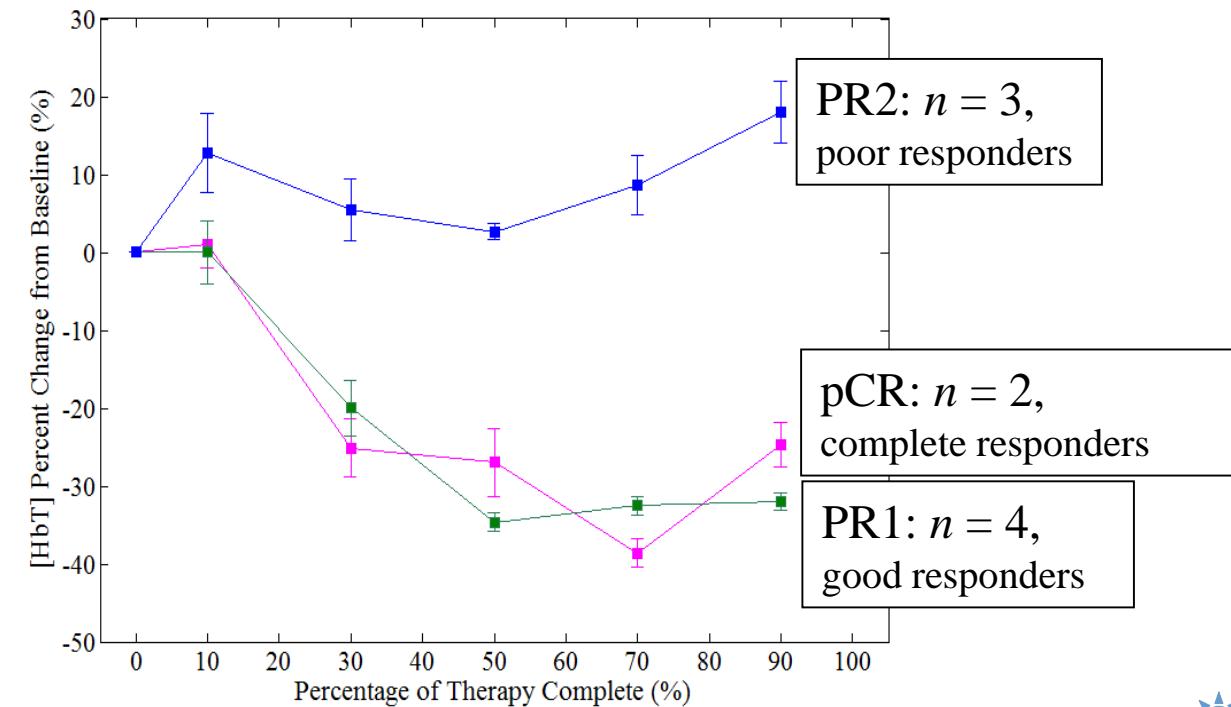


# [HbT] response to therapy: Representative Case (NACP #5) and group results

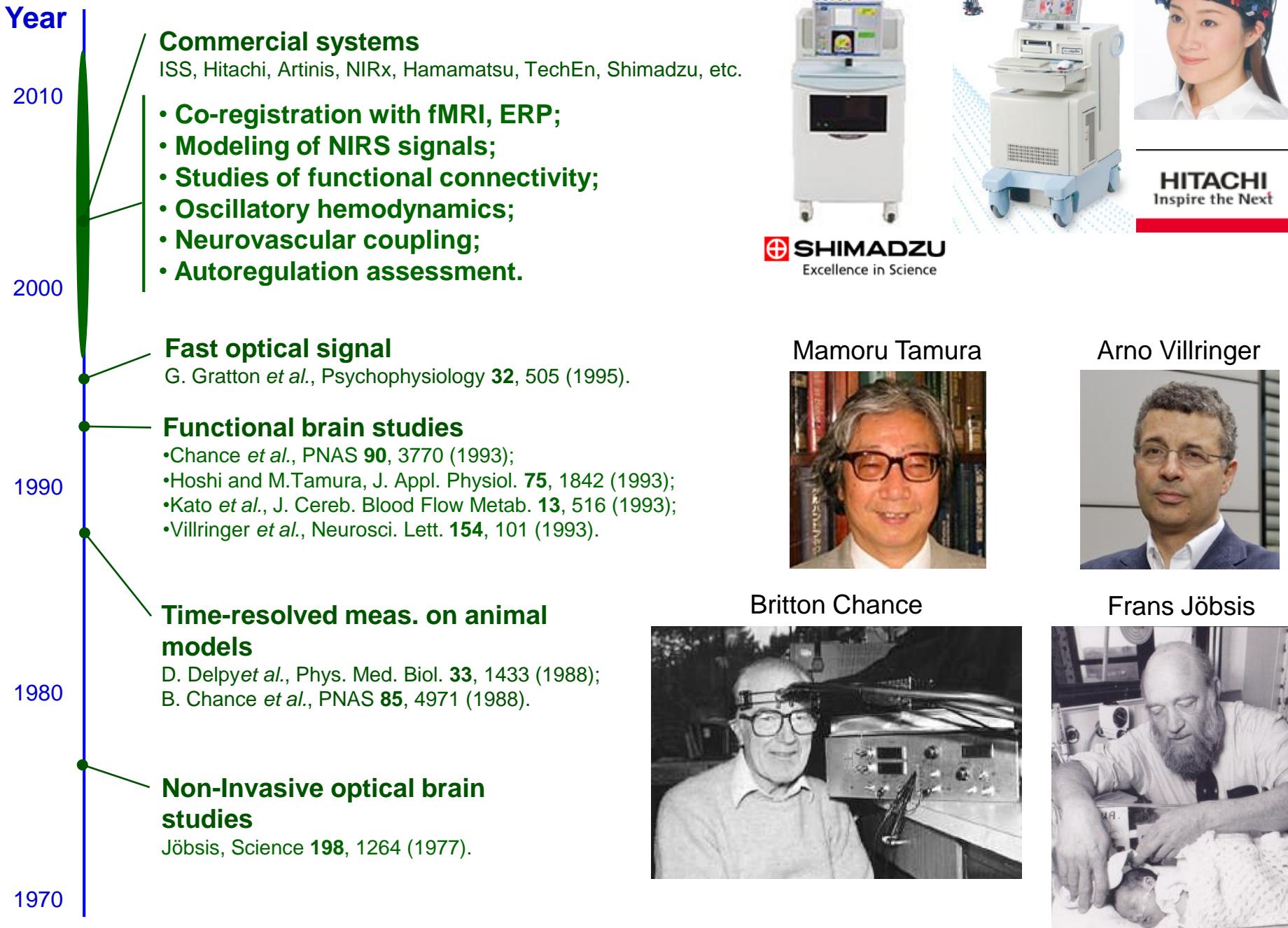


Age (years)	46
Type	Invasive ductal carcinoma
Max size (cm)	4.4
Response	pCR

Cancerous Breast [HbT] Response to Therapy: Group Results



# Non-invasive optical imaging of the brain

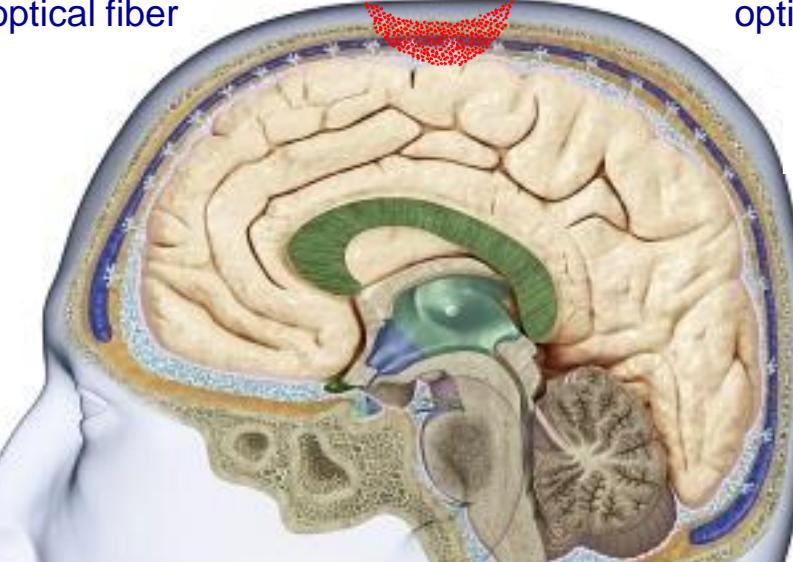


# Diffuse optical imaging of the human brain

Light source



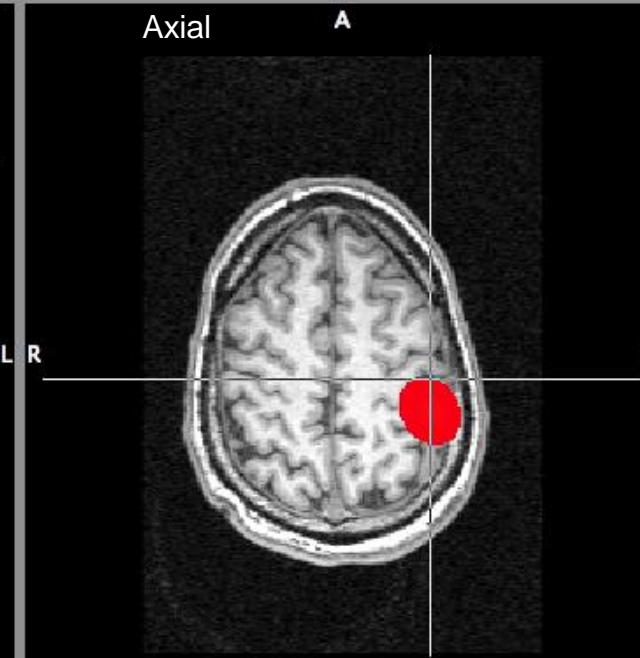
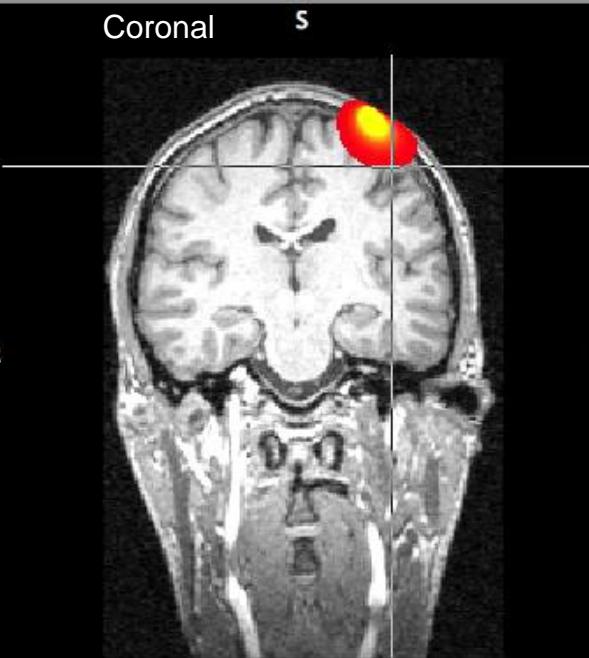
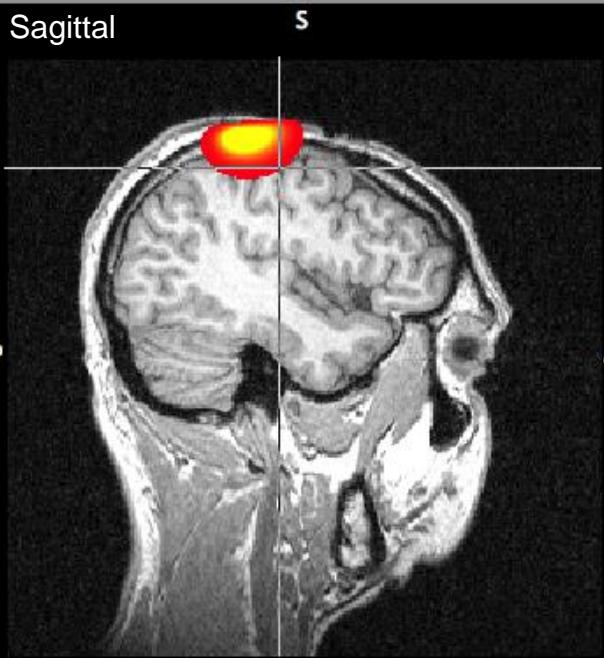
Illumination  
optical fiber

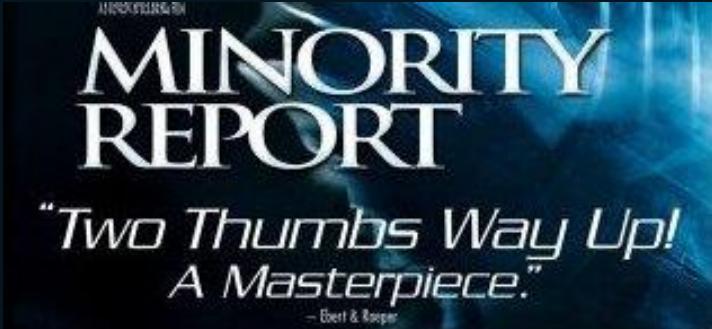


Collection  
optical fiber



Optical detector



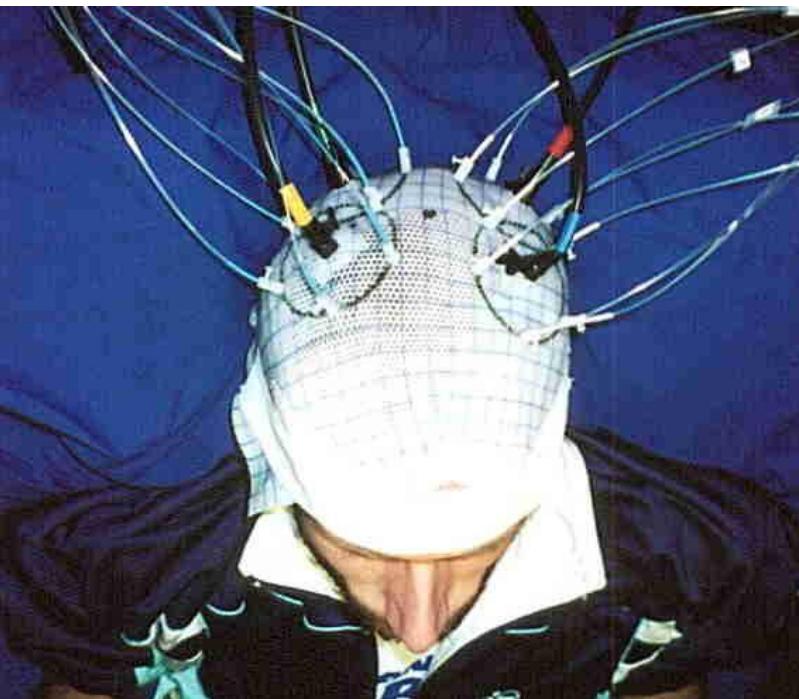


Steven Spielberg *et al.*, 2002.

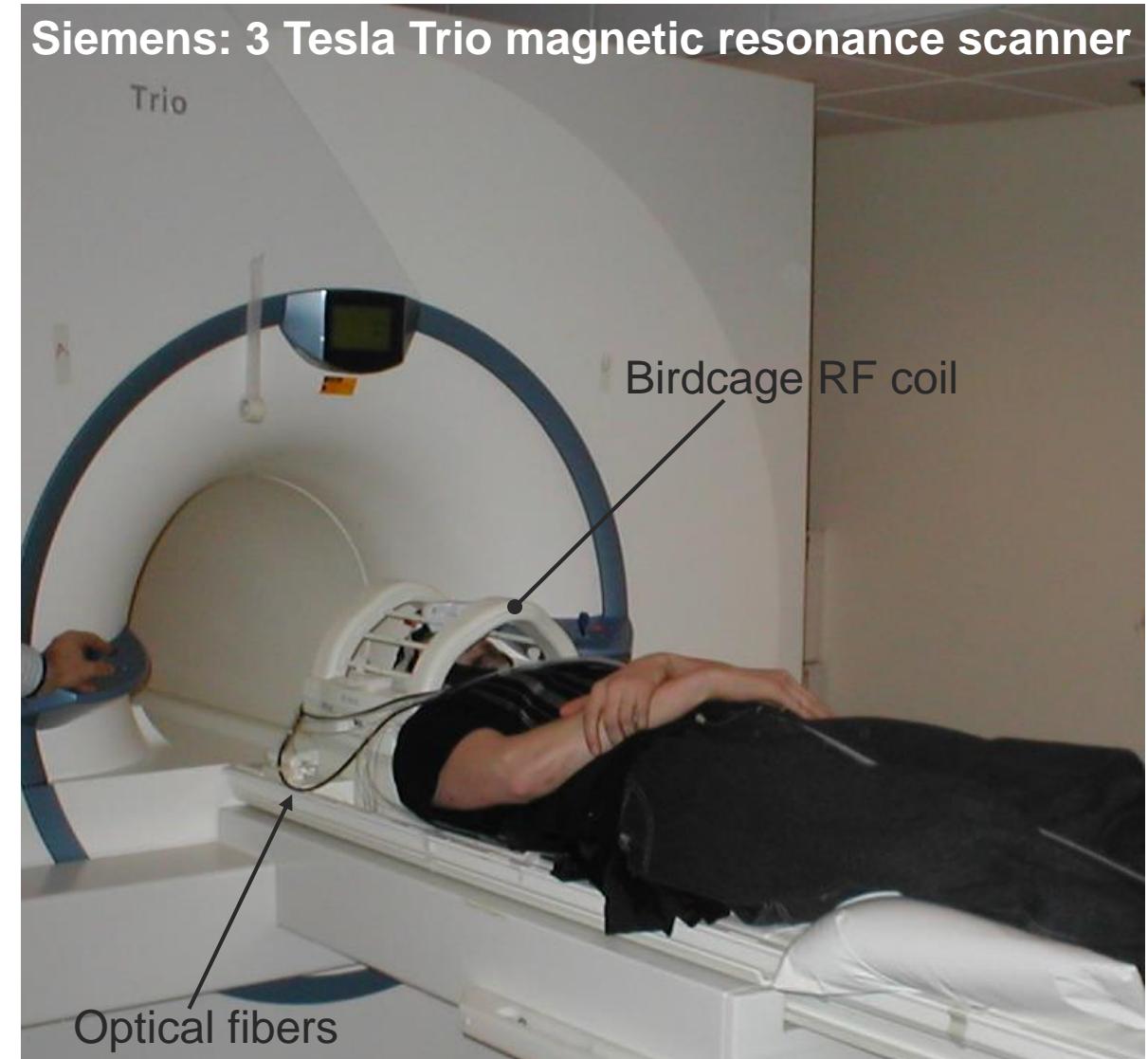


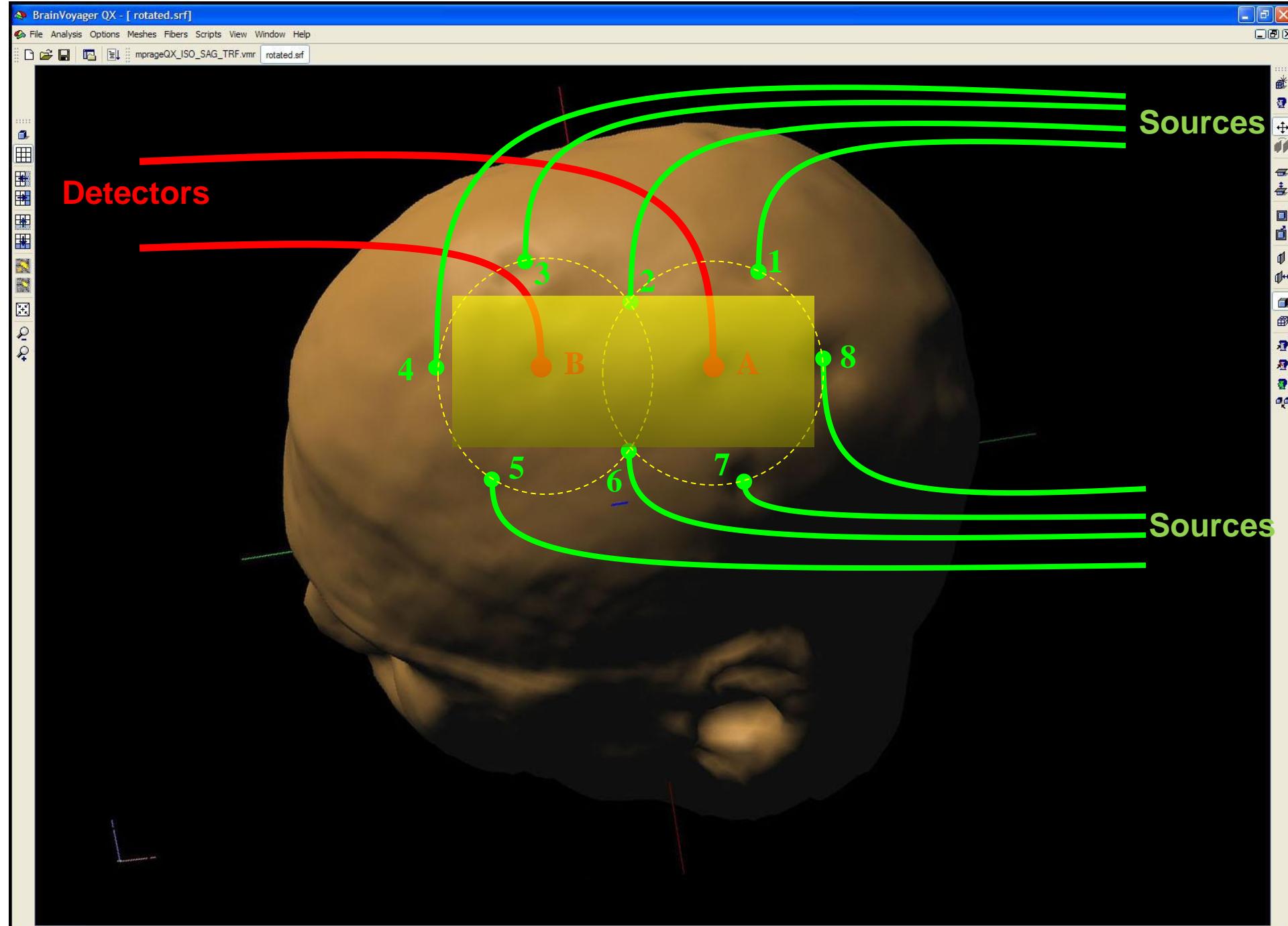
# Functional optical imaging of the brain at Tufts:

Concurrent fNIRS and fMRI (with B. Frederick, McLean Hospital, Belmont, MA)

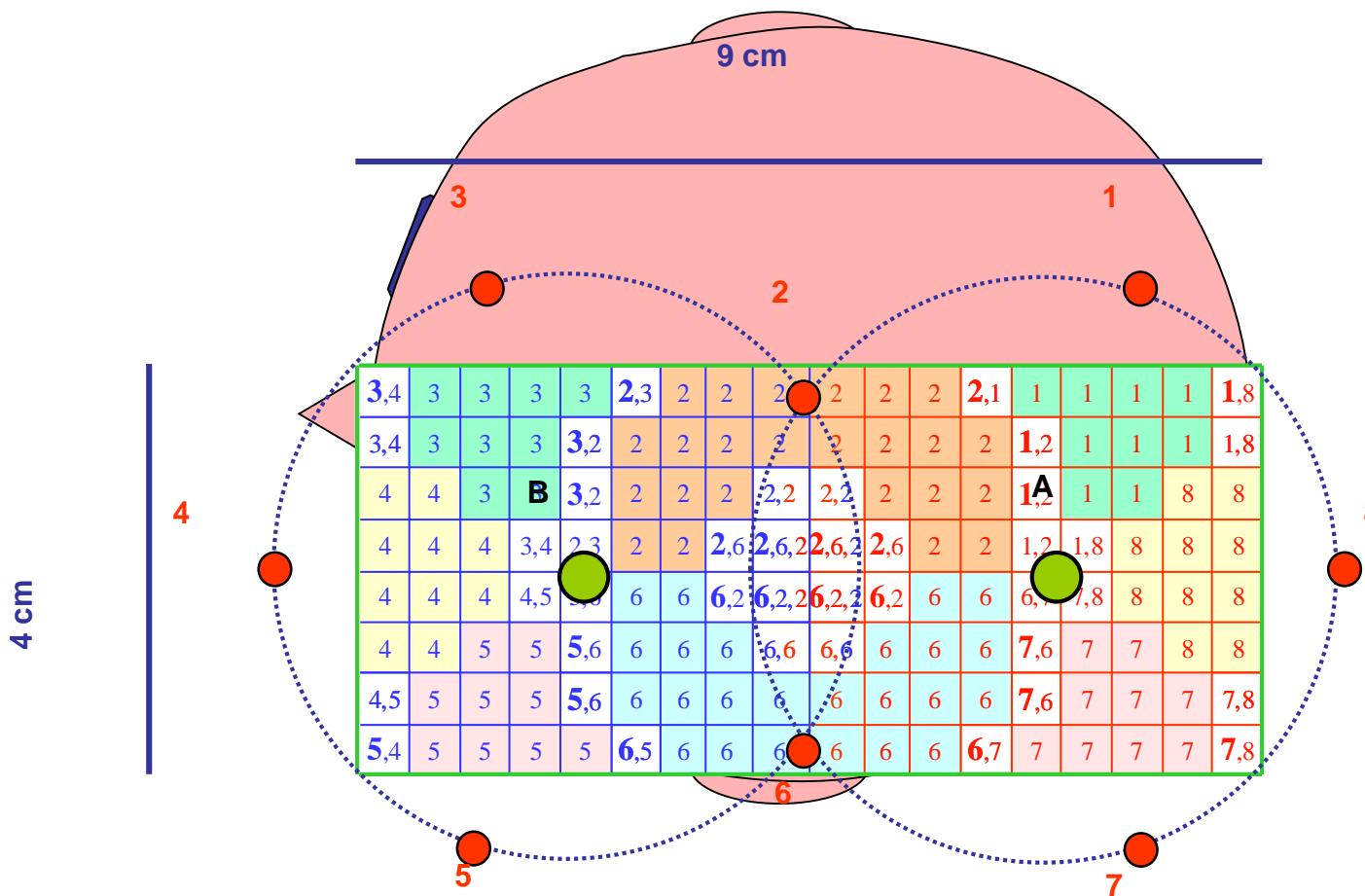


[Angelo Sassaroli, Yunjie Tong *et al.*, *NeuroImage* 33, 505 (2006)]

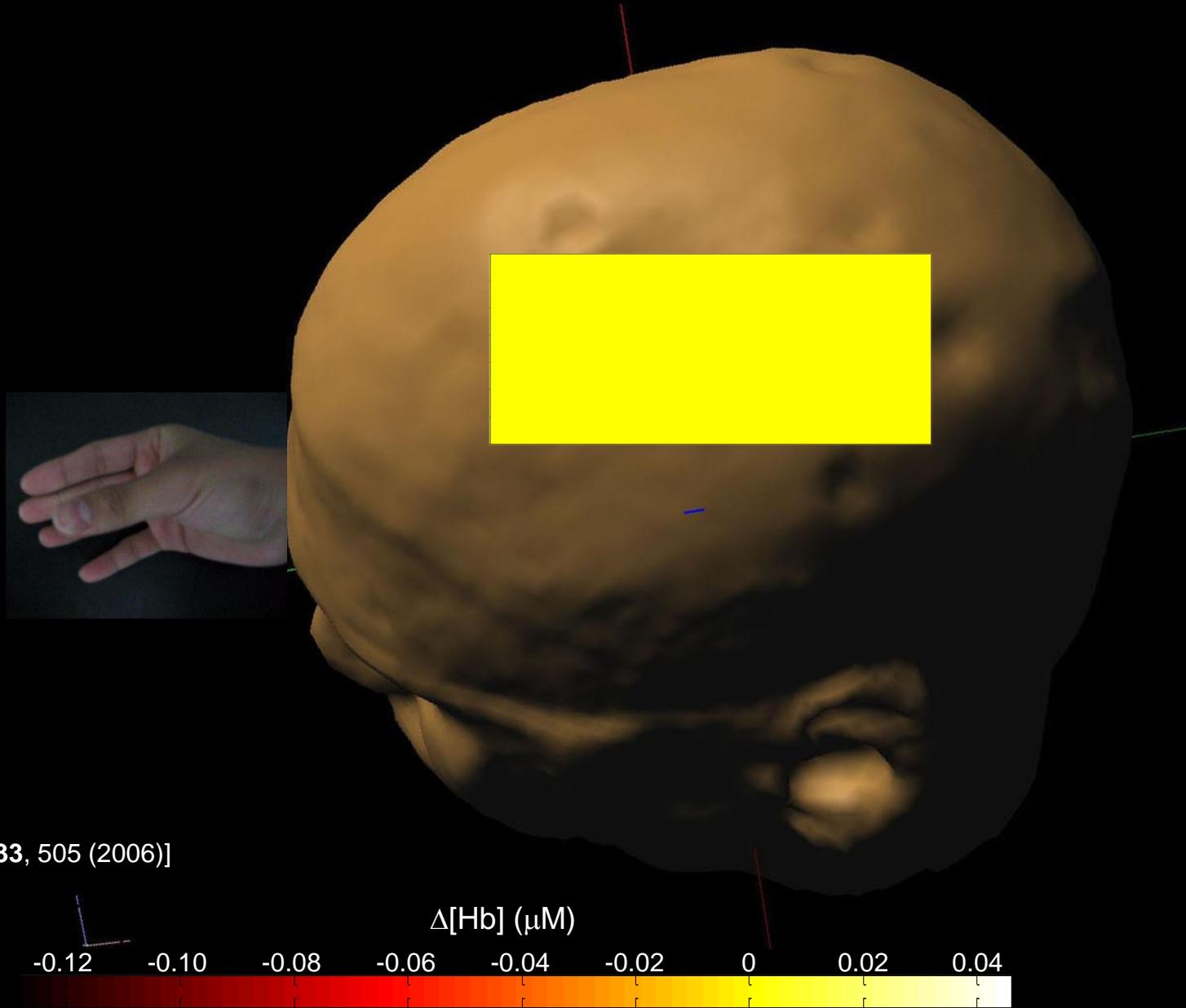




# Back-projection reconstruction matrix



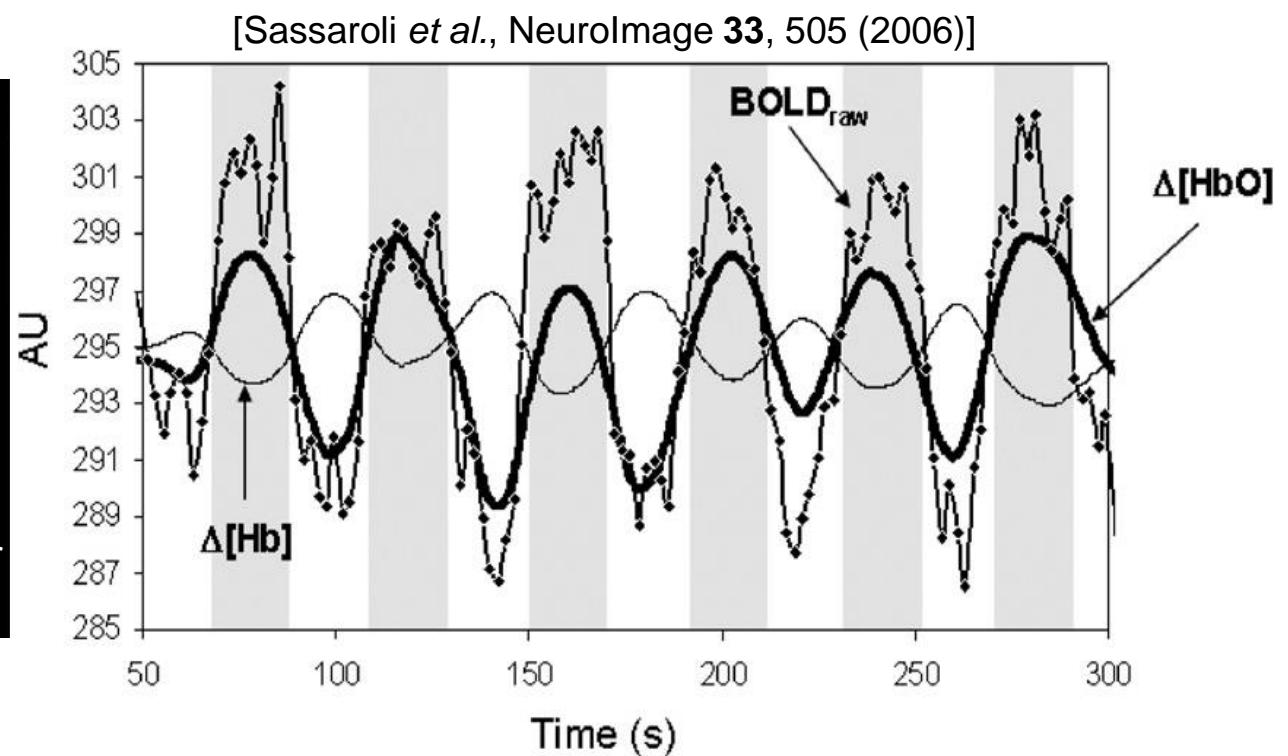
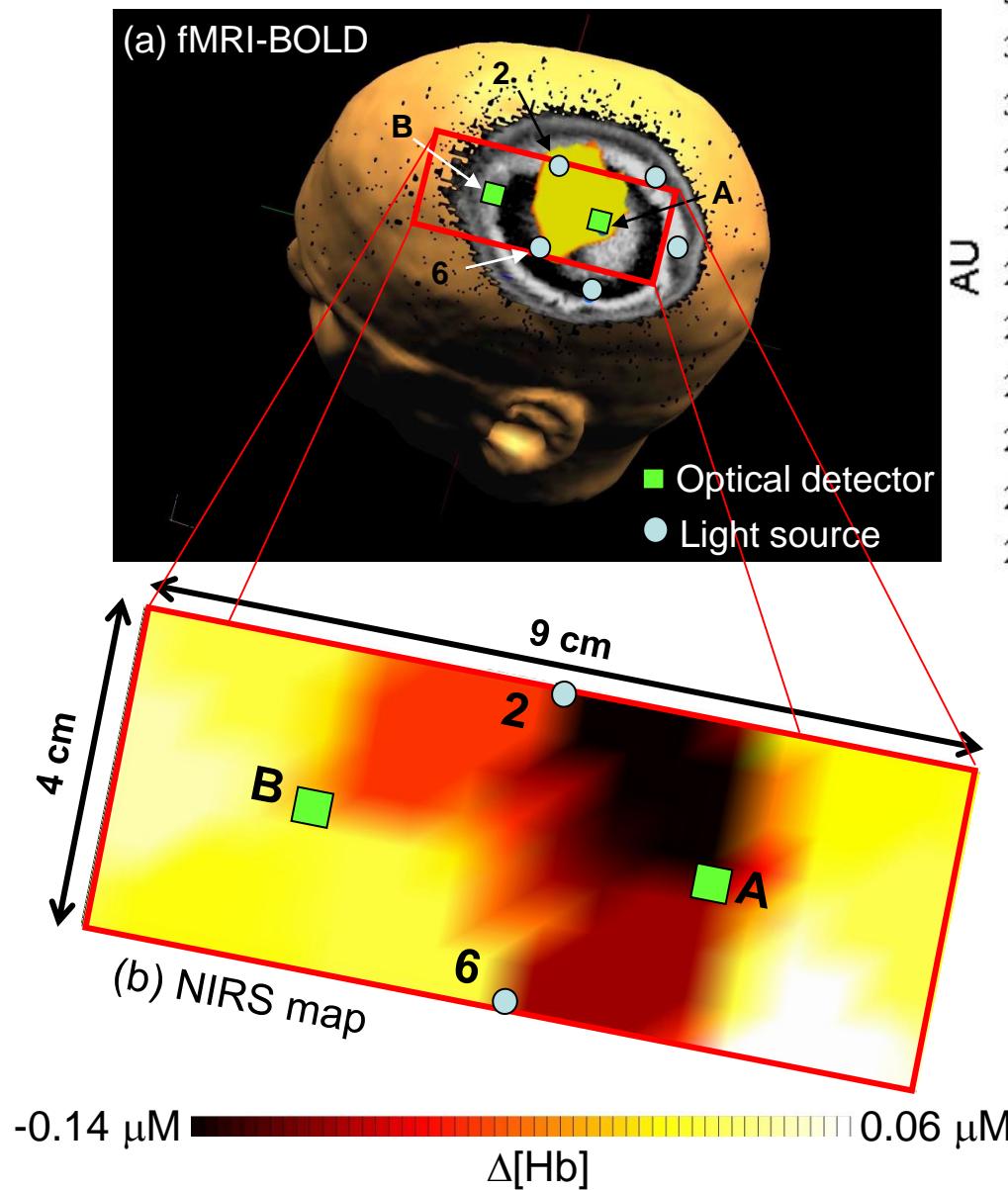
# Deoxy-hemoglobin concentration map during finger tapping



# Spatial and temporal comparison of fMRI-BOLD and NIRS mapping

(In collaboration with B. Frederick, McLean Hospital, Belmont, MA)

## Right hand tapping



$$\Delta[\text{Hb}]^{(\text{tissue})} \propto A \left( \frac{\Delta\sigma_{\text{bv}}}{\sigma_{\text{bv}}} \right) + B \left( \frac{\Delta\alpha_{\dot{\text{O}}_2}}{\alpha_{\dot{\text{O}}_2}} - \frac{\Delta c^{(\text{blood})}}{c^{(\text{blood})}} \right)$$

↑ Blood volume      ↑ Metabolic rate of oxygen      ↑ Blood flow velocity

[S. Fantini, *Phys. Med. Biol.* **47**, N249 (2002)]

[S. Fantini, *NeuroImage* **85**, 202 (2014)]

[S. Fantini, *Physiol. Meas.* **35**, N1 (2014)]

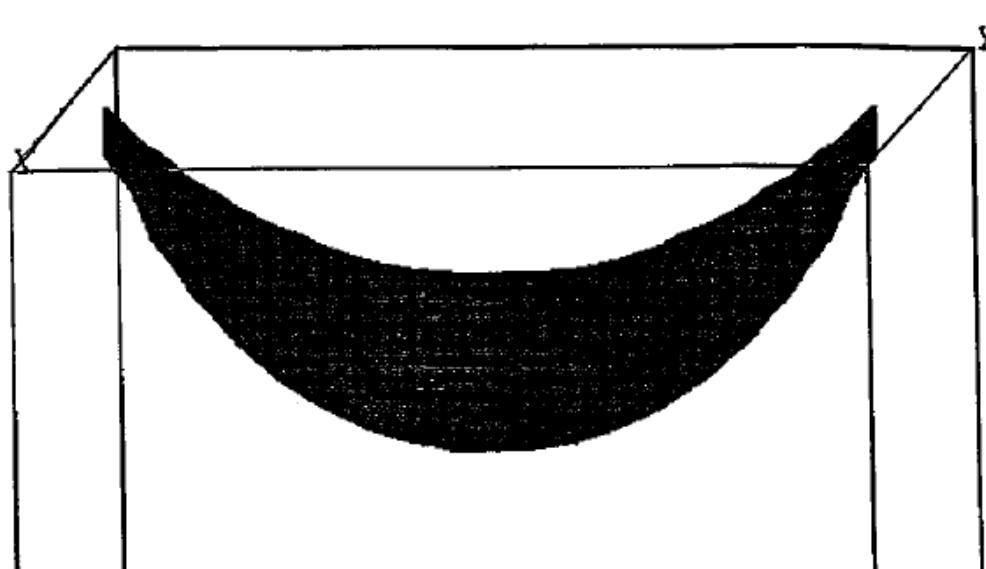
# The region of sensitivity in diffuse optics

Photon hitting density: J. Schotland et al, Appl. Opt. **32**, 448 (1993)

Photon-measurement density: S. Arridge, Appl. Opt. **34**, 7395 (1995)

$$J_p^{(M)}(\mathbf{r}_m, \mathbf{q}; \mathbf{r}')$$

$$\triangleq \lim_{\Delta p \rightarrow 0} \frac{F^{(M)}[\mathbf{r}_m, \mathbf{q}; \mathbf{p} + \Delta \mathbf{p}(\mathbf{r}')] - F^{(M)}[\mathbf{r}_m, \mathbf{q}; \mathbf{p}]}{\Delta \mathbf{p}(\mathbf{r}')} . \quad [\text{Arridge, Appl. Opt. } \mathbf{34}, 7395 \text{ (1995)}]$$



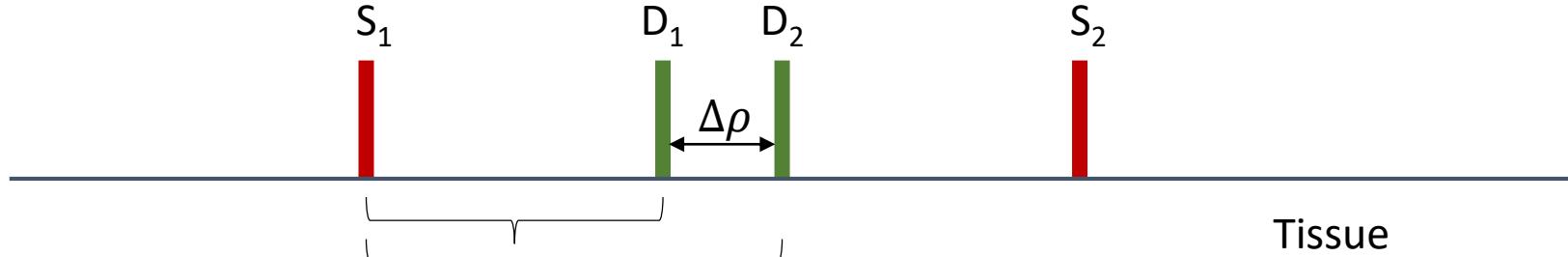
[Feng et al, Appl. Opt. **34**, 3826 (1995)]



# Dual slope of phase (or intensity)

Single slope 1:

$$Sl_{\varphi_1} = \sqrt{\frac{3\mu_a\mu'_s}{2}} \sqrt{\sqrt{1 + \left(\frac{\omega}{c_n\mu_a}\right)^2} - 1 + \frac{\varphi_{D2} - \varphi_{D1}}{\Delta\rho}}$$



Single slope 2:

$$Sl_{\varphi_2} = \sqrt{\frac{3\mu_a\mu'_s}{2}} \sqrt{\sqrt{1 + \left(\frac{\omega}{c_n\mu_a}\right)^2} - 1 + \frac{\varphi_{D1} - \varphi_{D2}}{\Delta\rho}}$$

Dual slope:

$$DSl_{\varphi} = \frac{Sl_{\varphi_1} + Sl_{\varphi_2}}{2} = \sqrt{\frac{3\mu_a\mu'_s}{2}} \sqrt{\sqrt{1 + \left(\frac{\omega}{c_n\mu_a}\right)^2} - 1}$$

[Hueber et al, Proc. SPIE 3597, 618-631 (1999)]

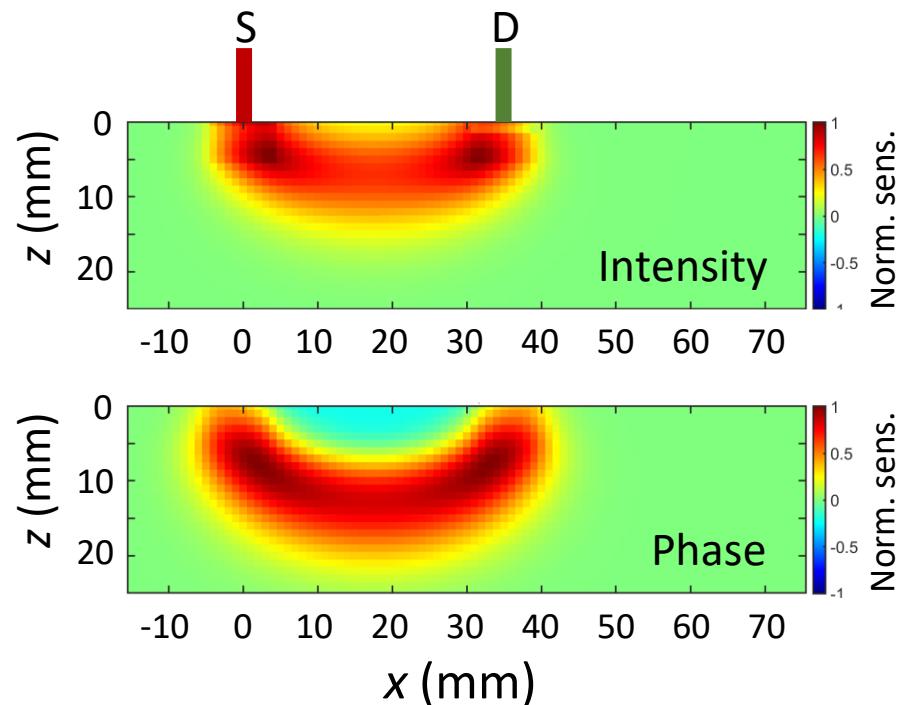


# Region of sensitivity for intensity and phase measurements

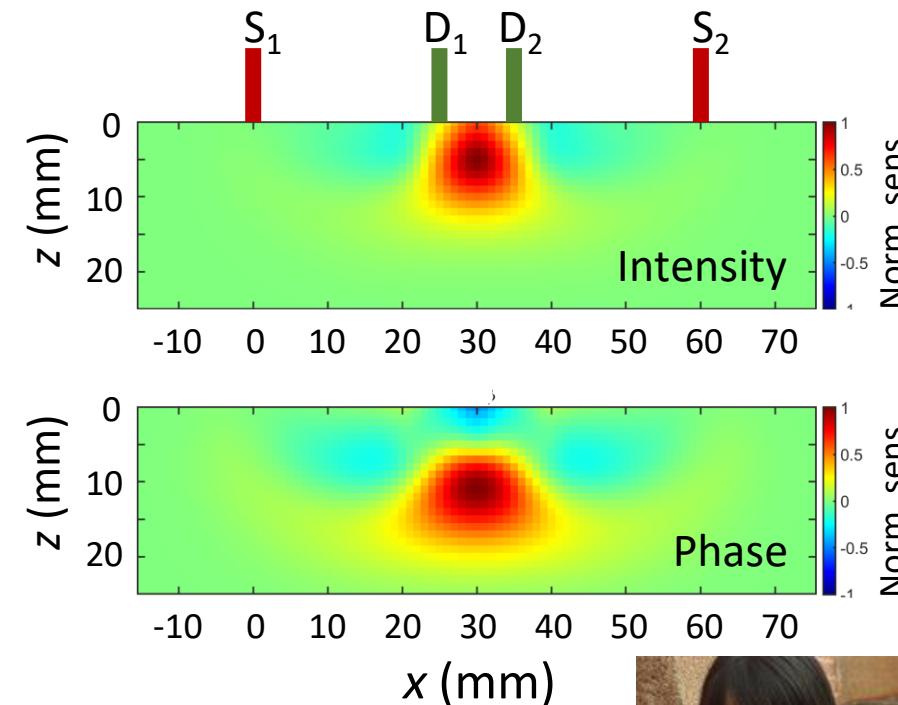
## Single-Distance, Dual-Slope

$$\begin{aligned}\mu_{a0} &= 0.1 \text{ cm}^{-1} \\ \mu'_s &= 12 \text{ cm}^{-1} \\ \Delta\mu_a &= 0.03 \text{ cm}^{-1} \\ \Delta V &= 0.7 \text{ cm}^3\end{aligned}$$

Single-distance (1S-1D)



Dual-slope (2S-2D)

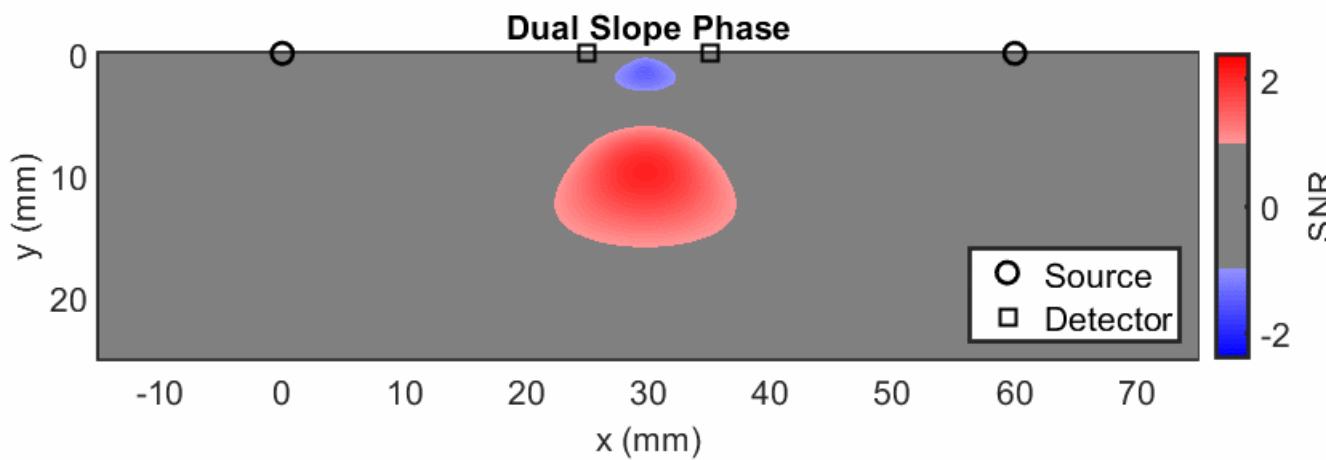
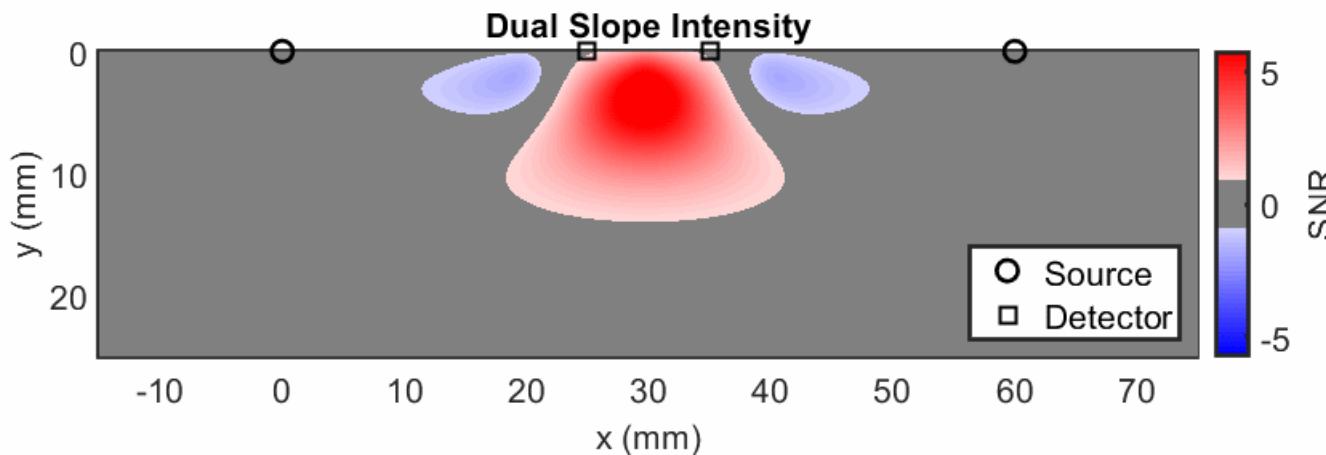


[Giles Blaney et al., J. Biophotonics (*submitted, 2019*)]

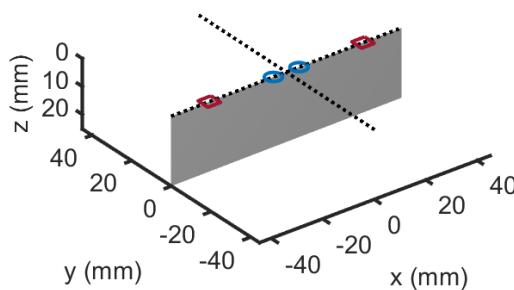
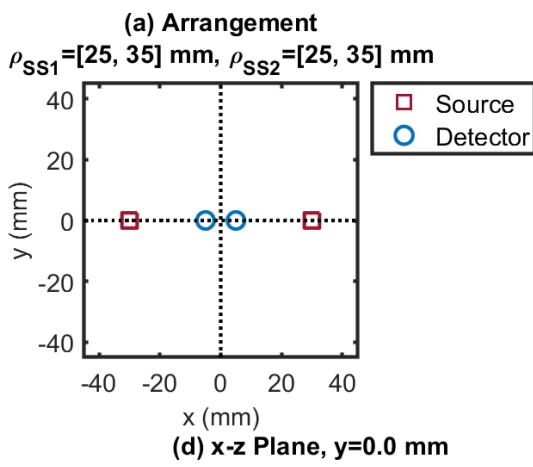
[Angelo Sassaroli et al., J. Opt. Soc. Am A (*submitted, 2019*)]



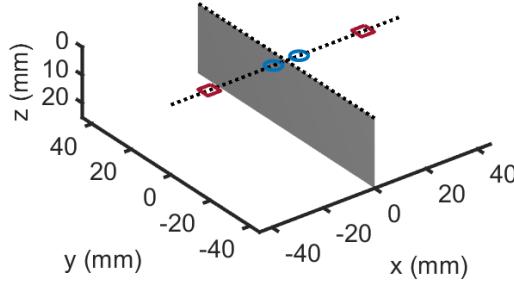
# Comparison of intensity and phase dual slopes



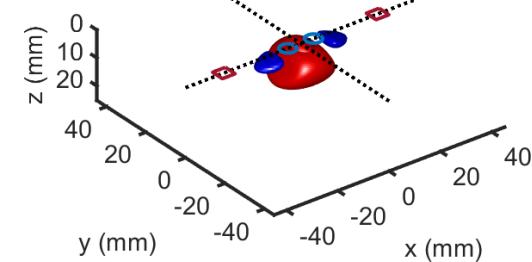
# Linear arrangement



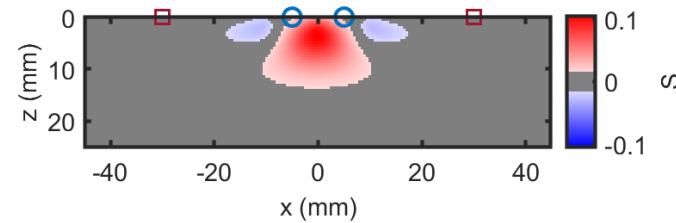
(g) y-z Plane,  $x=0.0 \text{ mm}$



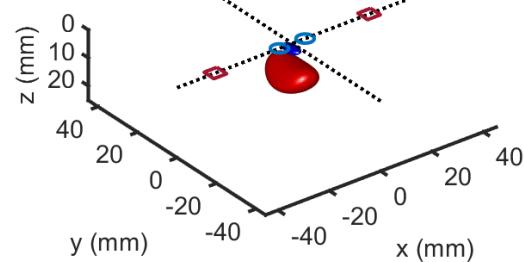
Intensity  
(b) DSI SNR=1 Surface



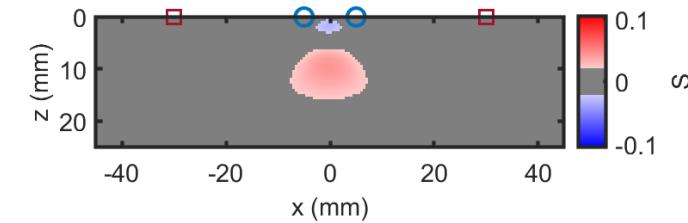
(e) DSI, x-z Plane,  $y=0.0 \text{ mm}$



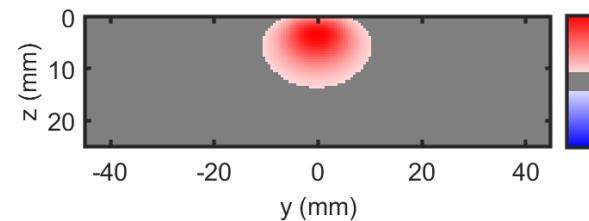
Phase  
(c) DS $\phi$  SNR=1 Surface



(f) DS $\phi$ , x-z Plane,  $y=0.0 \text{ mm}$



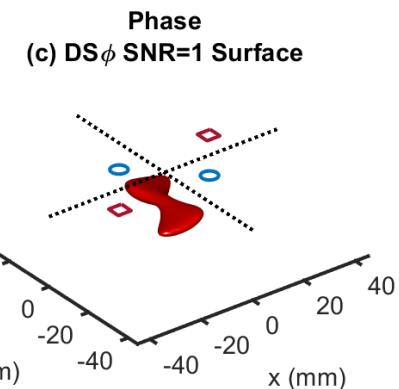
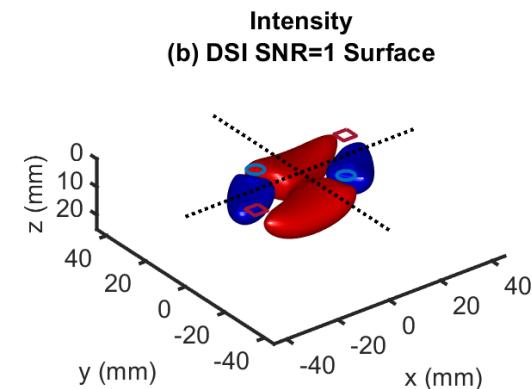
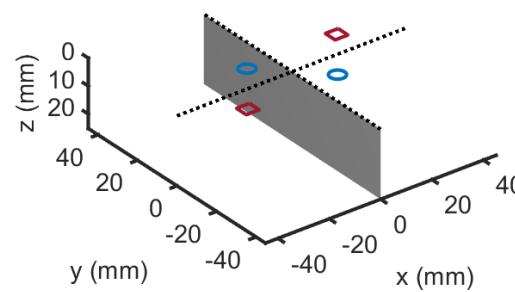
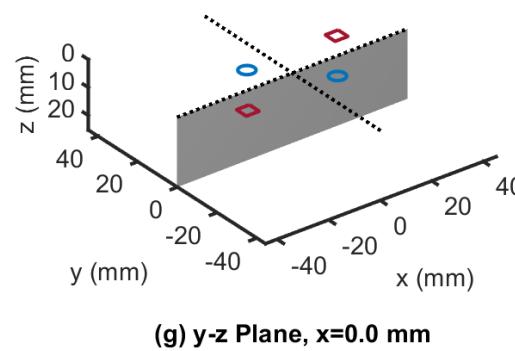
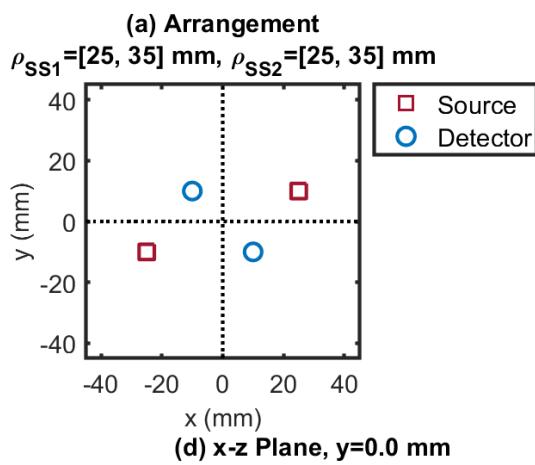
(h) DSI, y-z Plane,  $x=0.0 \text{ mm}$



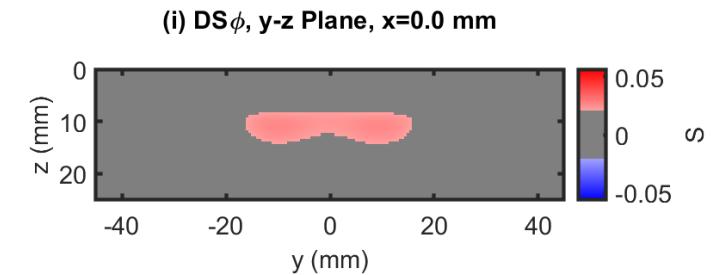
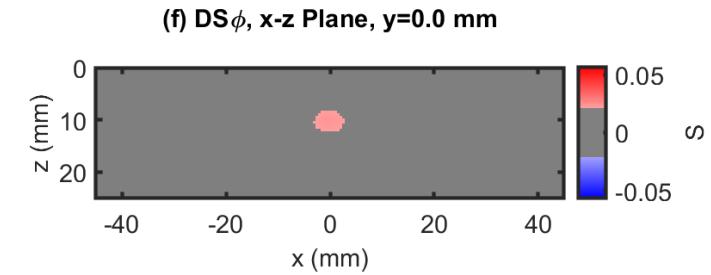
Hazelnut



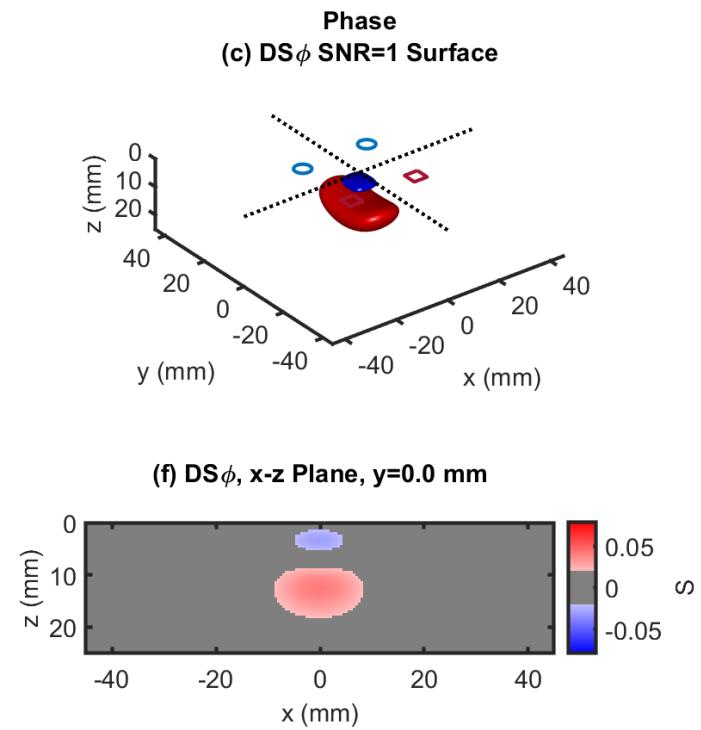
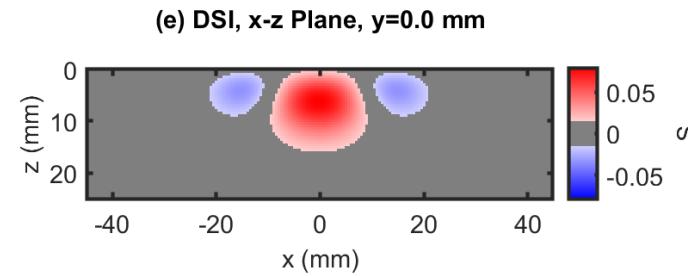
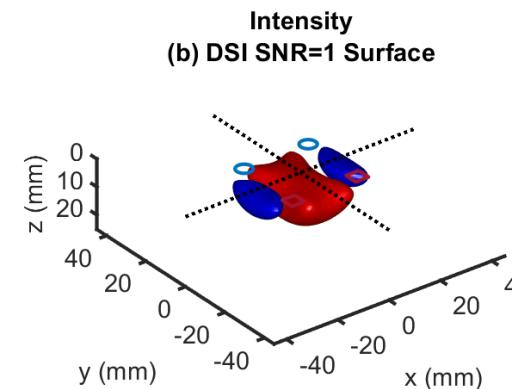
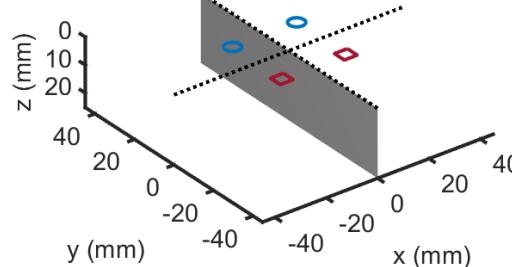
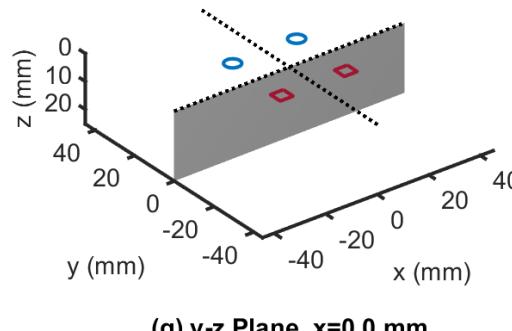
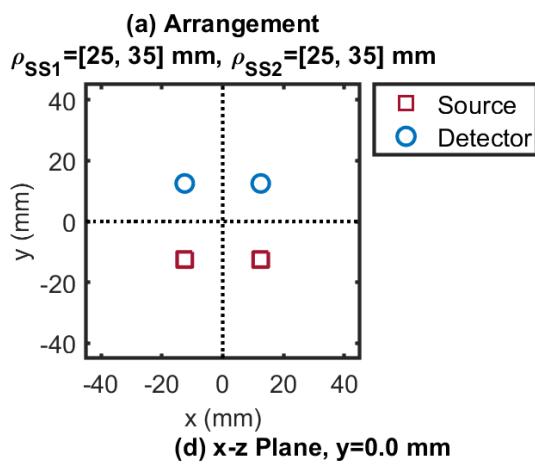
# Rhomboid arrangement



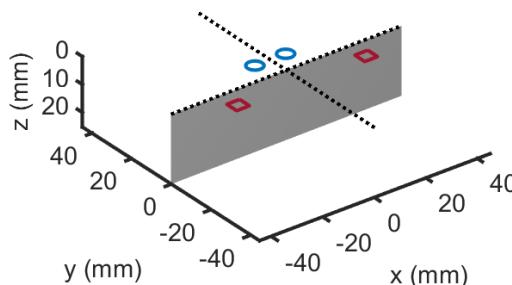
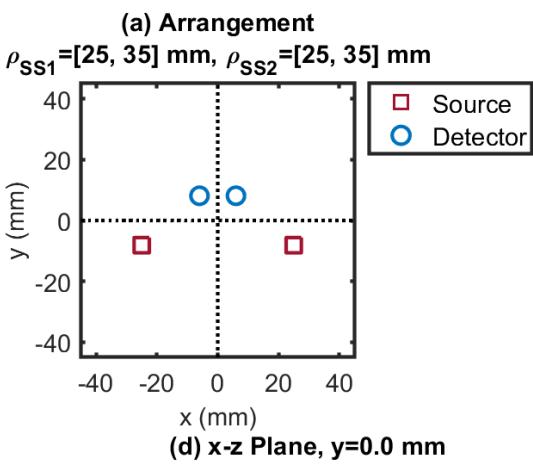
## Peanut



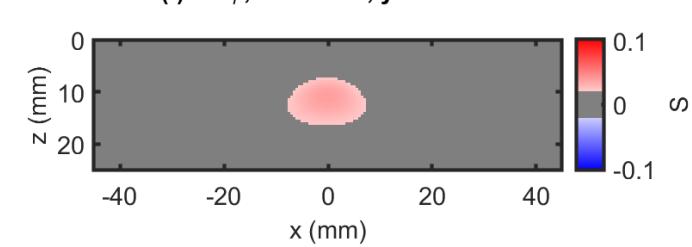
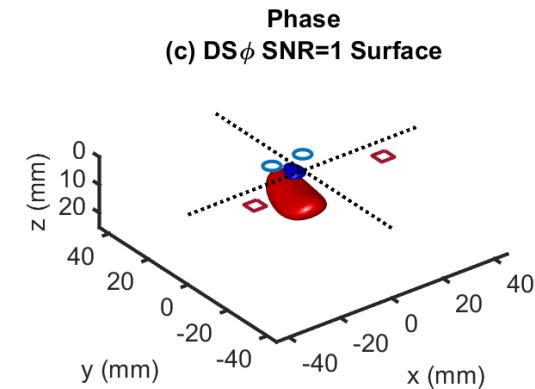
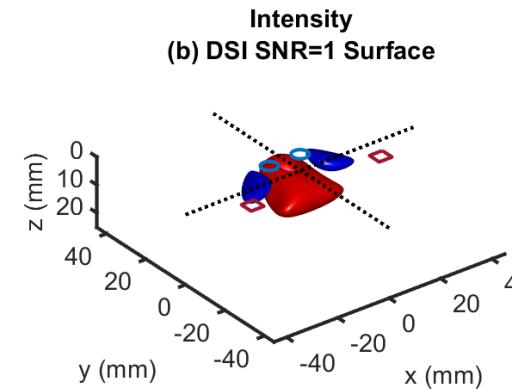
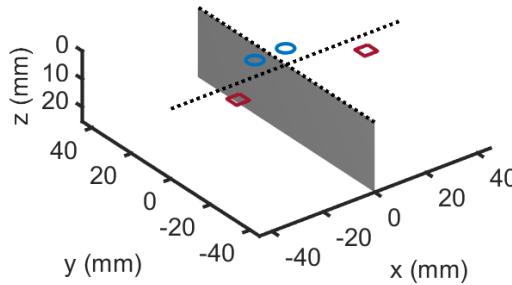
# Square arrangement



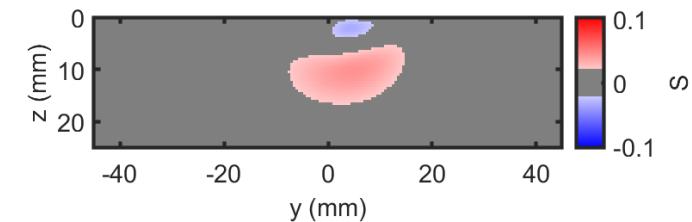
# Trapezoid arrangement



(g) y-z Plane,  $x=0.0 \text{ mm}$



(i) DS $\phi$ , y-z Plane,  $x=0.0 \text{ mm}$



Chestnut



# COMING SOON

Sergio Fantini, Giles Blaney, and Angelo Sassaroli

**“Transformational change in the field of diffuse optics:  
From going bananas to going nuts”**

J. Innovative Optical Health Sciences, SUBMITTED TODAY



# Conclusions

- **Diagnostic applications of diffuse optical imaging:**
  - Breast cancer imaging
  - Functional brain imaging
- **For researchers in the field of diffuse optics it is preferable going nuts than going bananas**



# MANY THANKS TO ALL “DOIT Lab” MEMBERS

